

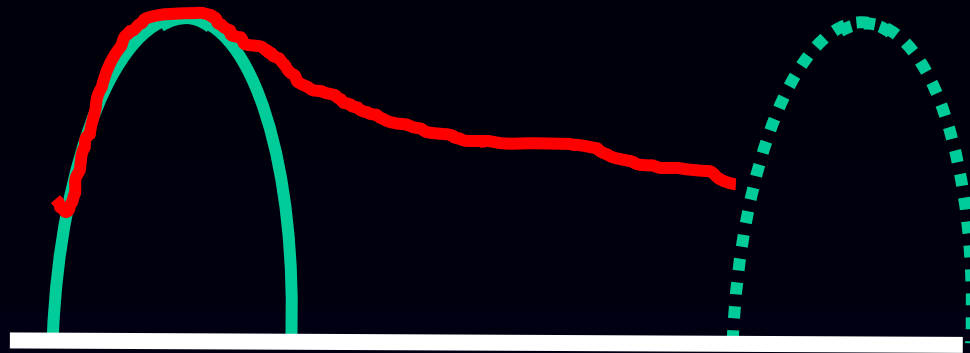
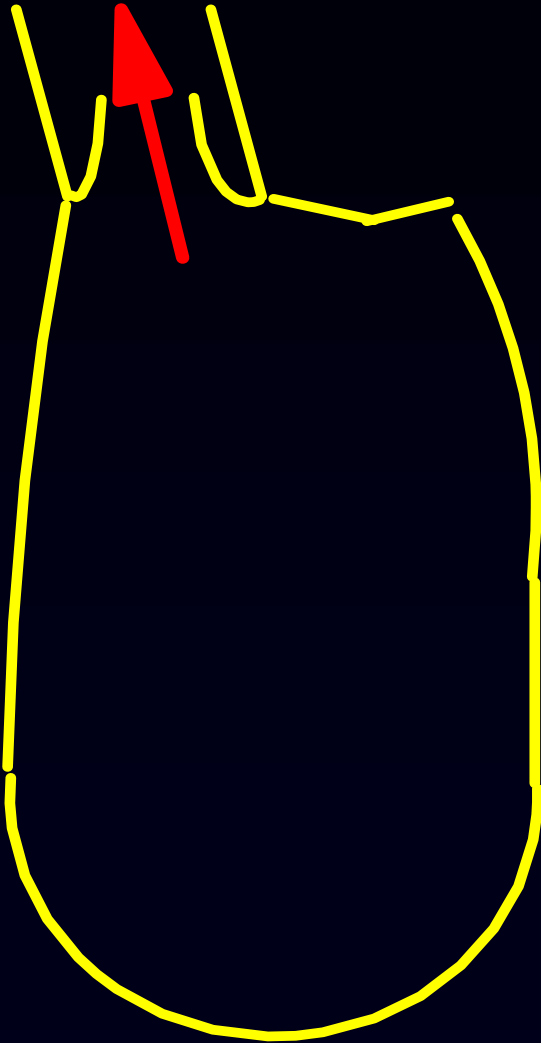
Les méthodes de pulse contour

Daniel De Backer
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Erasmus University Hospital
Brussels, Belgium

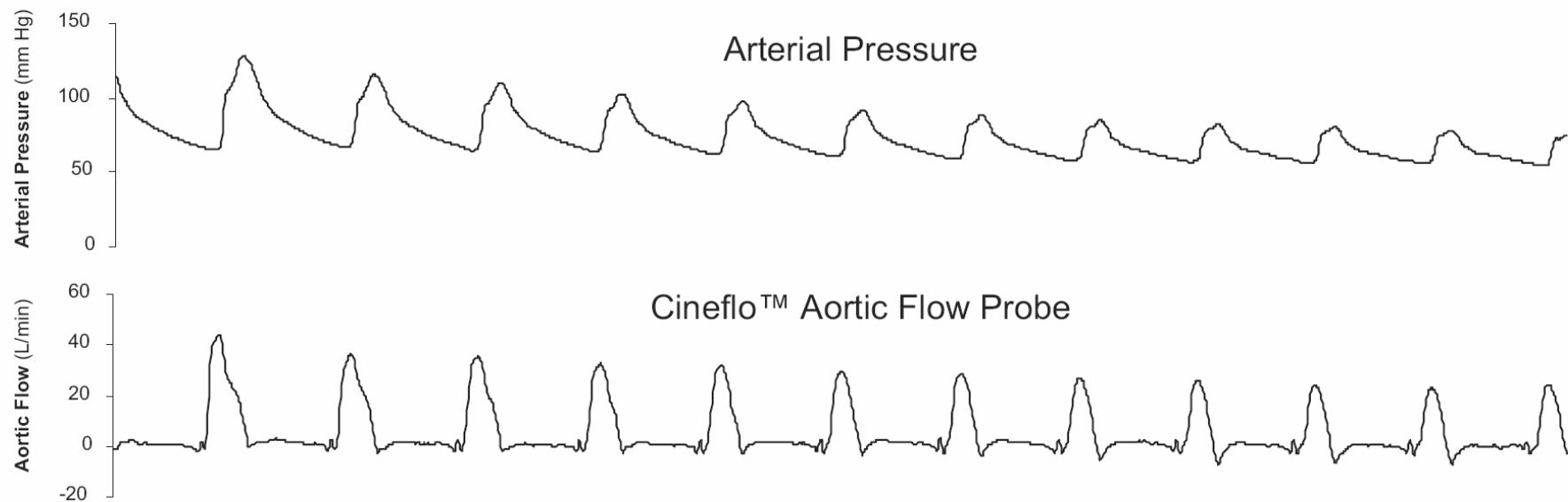
Pulse contour methods:

- **With calibration**
 - => **Transpulmonary thermodilution (PiCCO)**
 - => **Lithium dilution (LiDCO)**
- **Without calibration**
 - => **FloTrac**
 - => **PRAM**

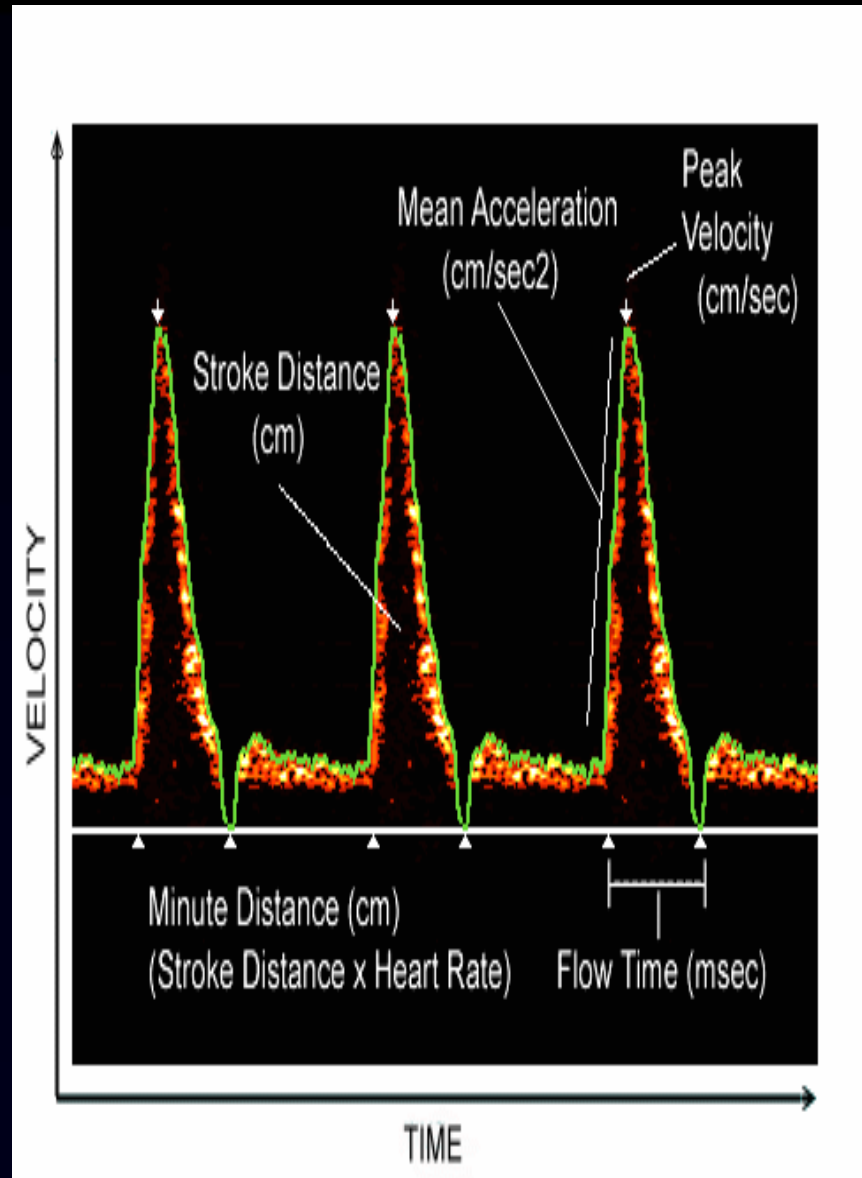
What is the link between stroke volume and arterial pressure ?



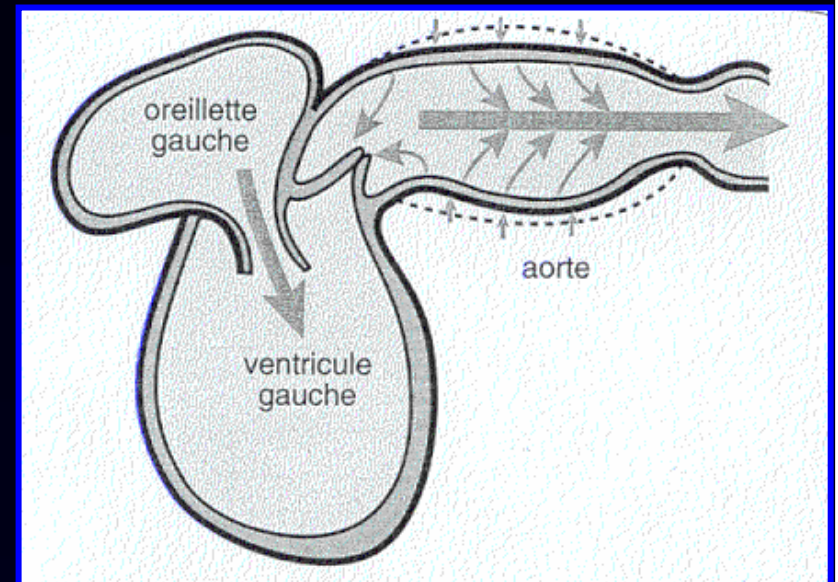
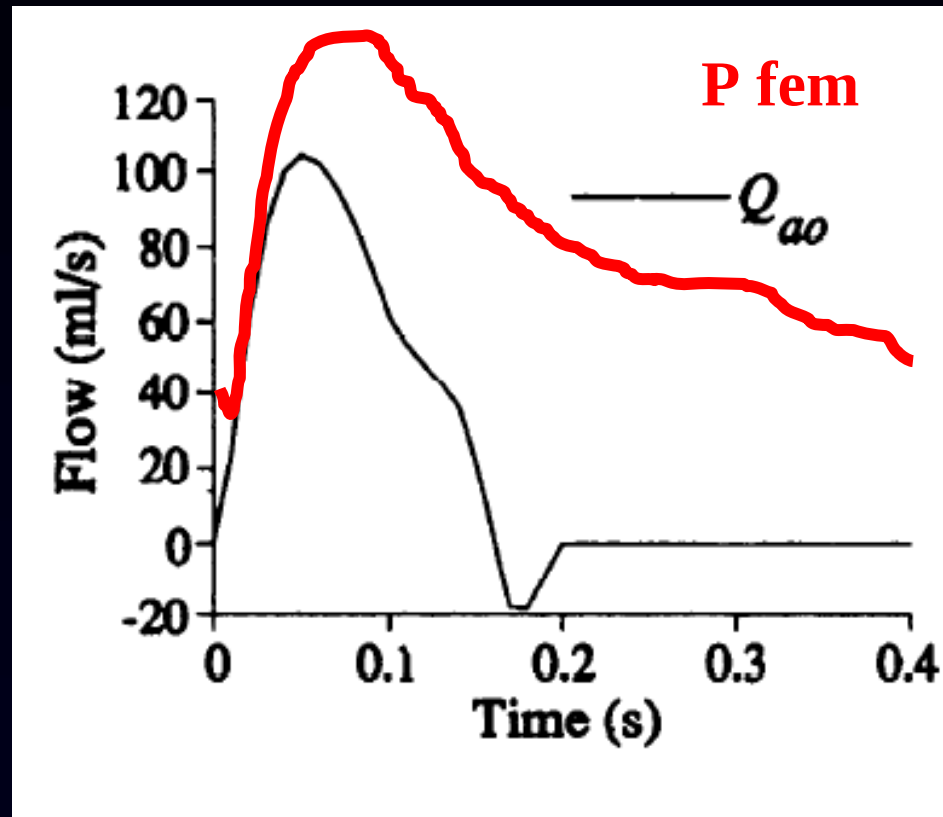
Effect of IVC Occlusion on Measured Hemodynamic Variables



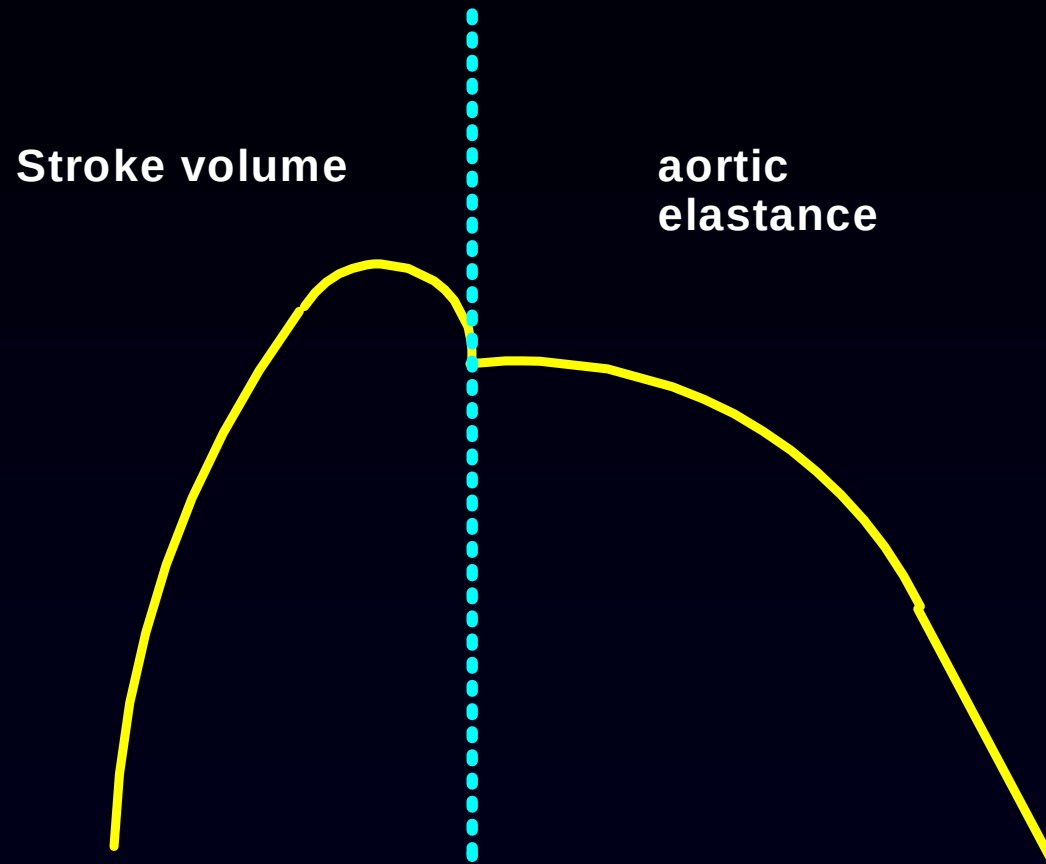
What is the link between stroke volume and arterial pressure ?



What is the link between stroke volume and arterial pressure ?

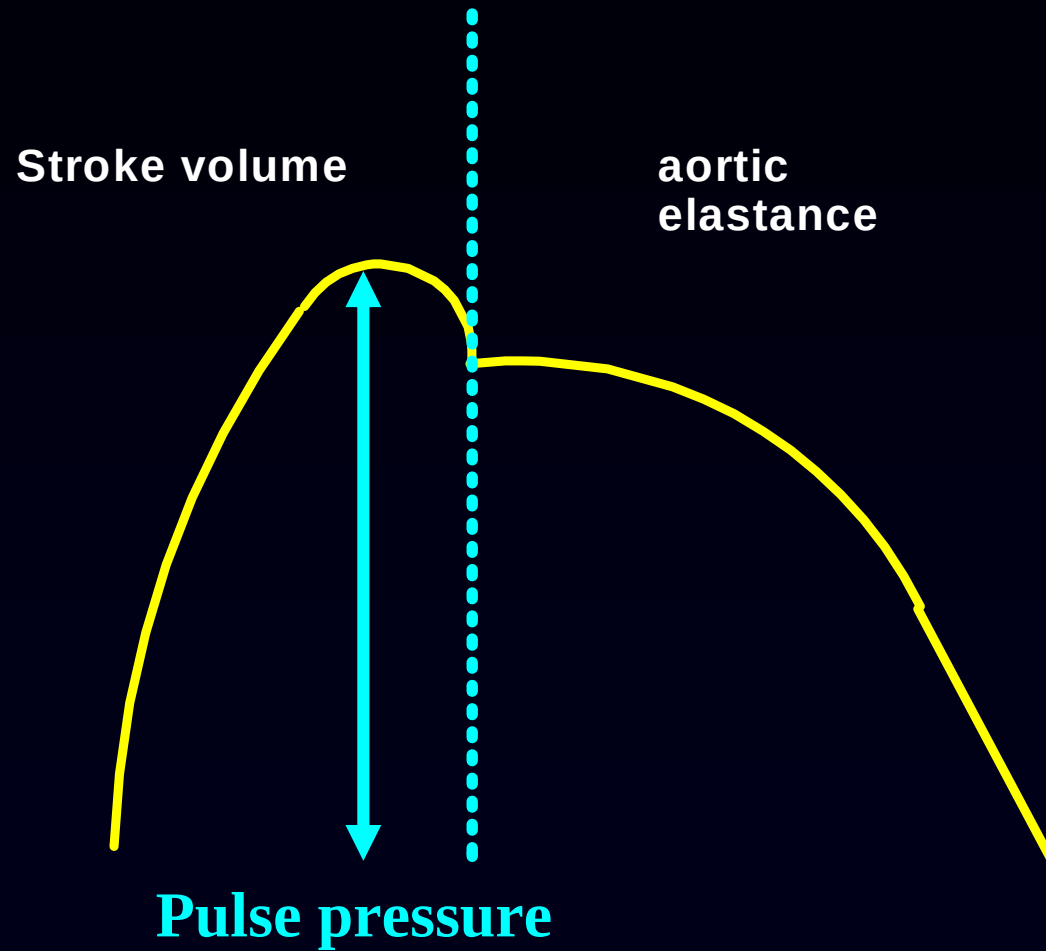


Factors influencing the arterial pressure curve



Pulse pressure ?

Factors influencing the arterial pressure curve

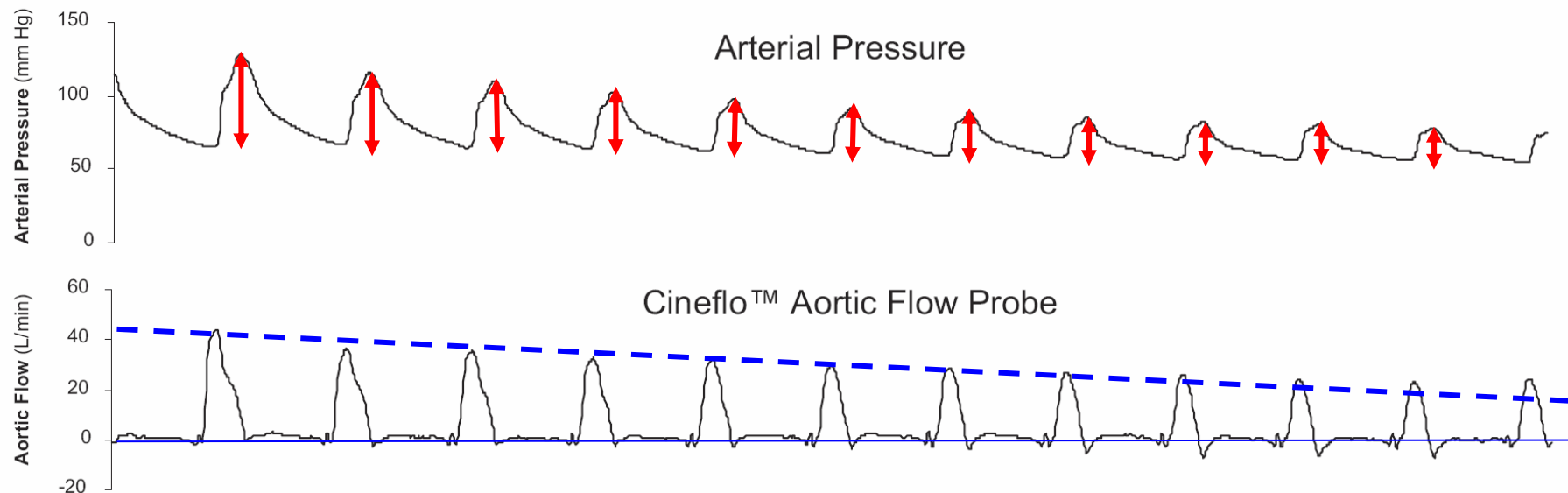


Ability of pulse power, esophageal Doppler and arterial pulse pressure to estimate rapid changes in stroke volume in humans

José Marquez, MD; Kenneth McCurry, MD; Donald A. Severyn, MS; Michael R. Pinsky, MD

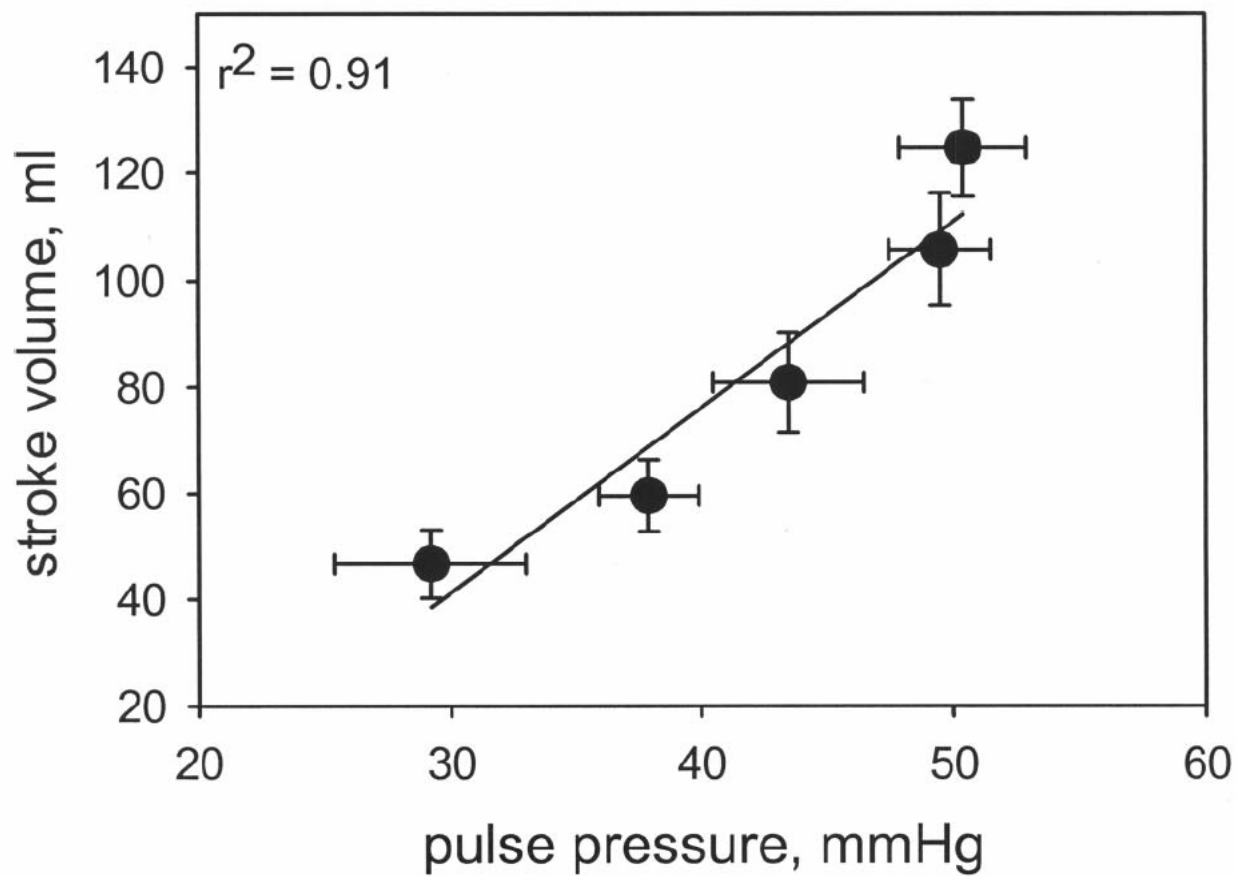
Marques et al
Crit Care Med 2008

Effect of IVC Occlusion on Measured Hemodynamic Variables



Arterial Pulse Pressure and Its Association With Reduced Stroke Volume During Progressive Central Hypovolemia

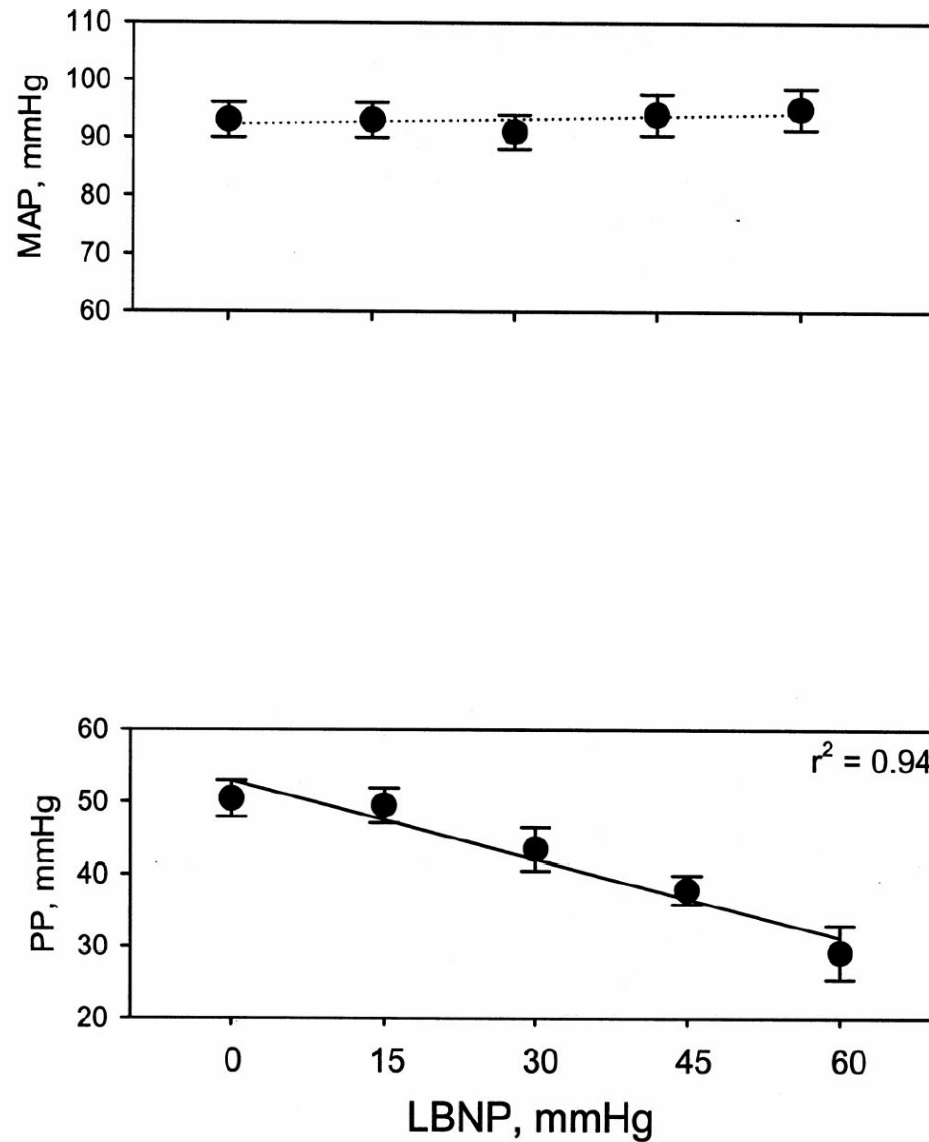
Victor A. Convertino, PhD, William H. Cooke, PhD, and John B. Holcomb, M.
J Trauma. 2006;61:629–634



Arterial Pulse Pressure and Its Association With Reduced Stroke Volume During Progressive Central Hypovolemia

Victor A. Convertino, PhD, William H. Cooke, PhD, and John B. Holcomb, MD

J Trauma. 2006;61:629–634



PA

artères
rigides

artères
normales

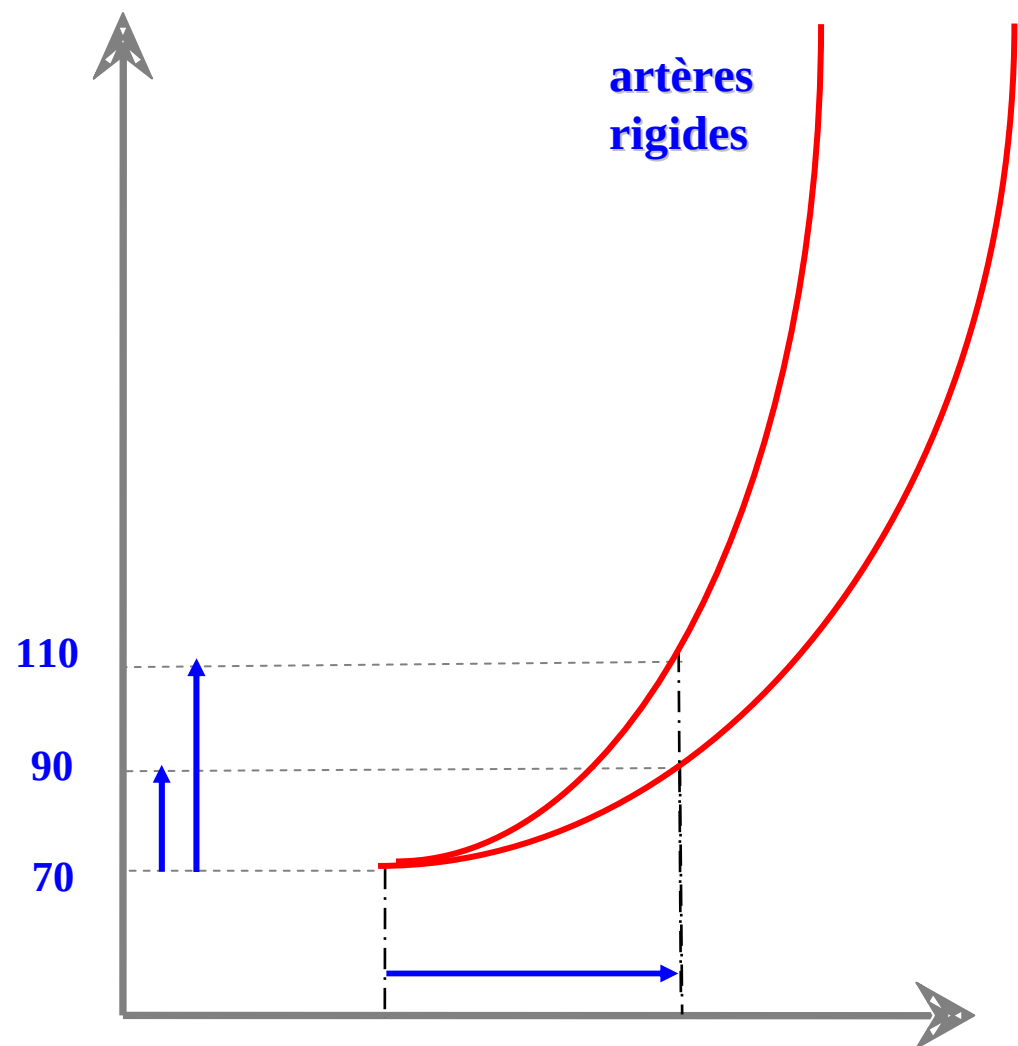
110

90

70

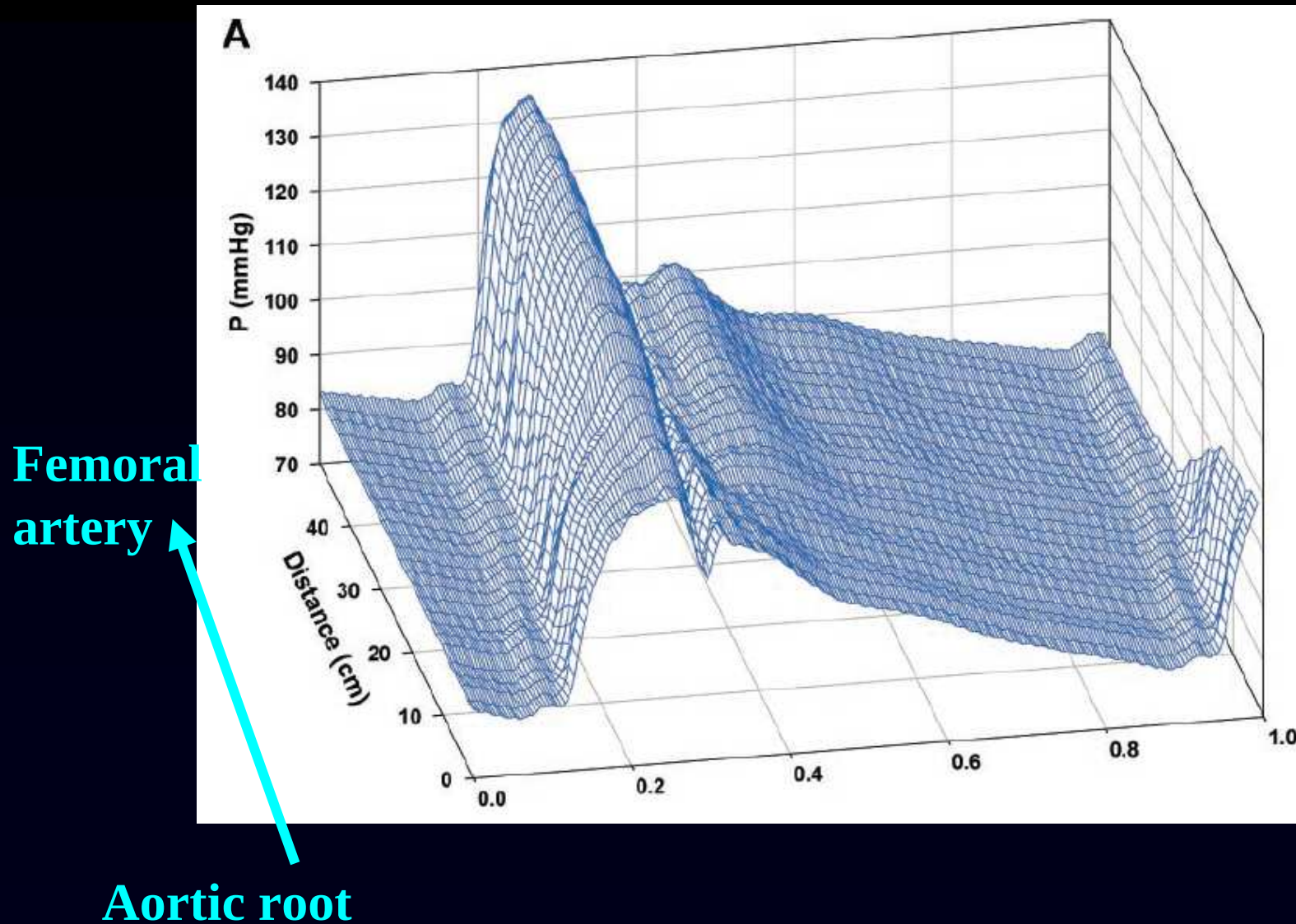
VES

volume



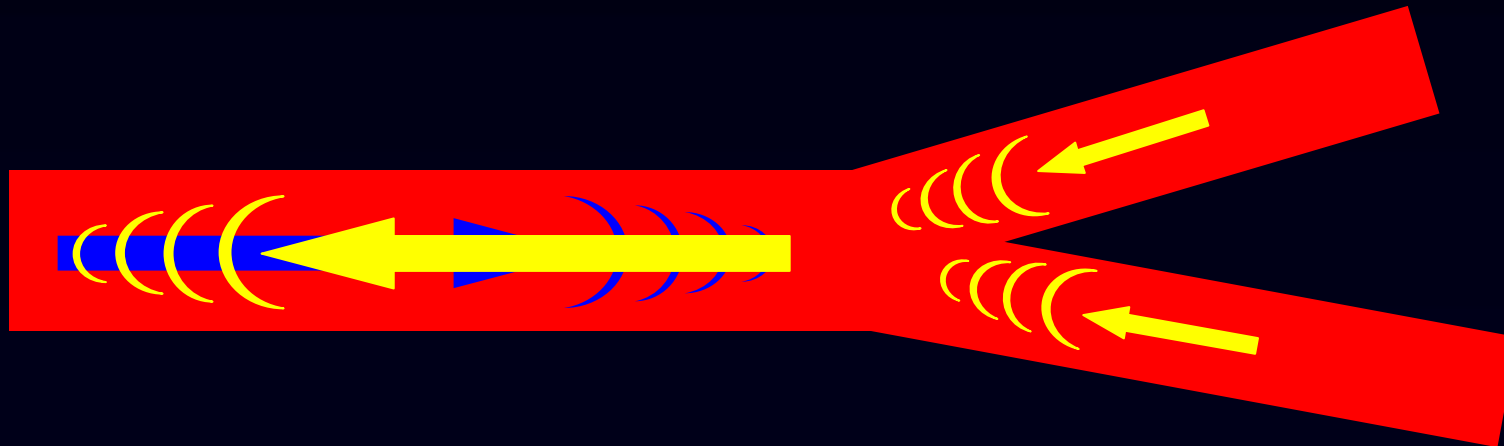
Distortion of the signal by reflected waves

Wang J et al
AJP 284:1358;2003

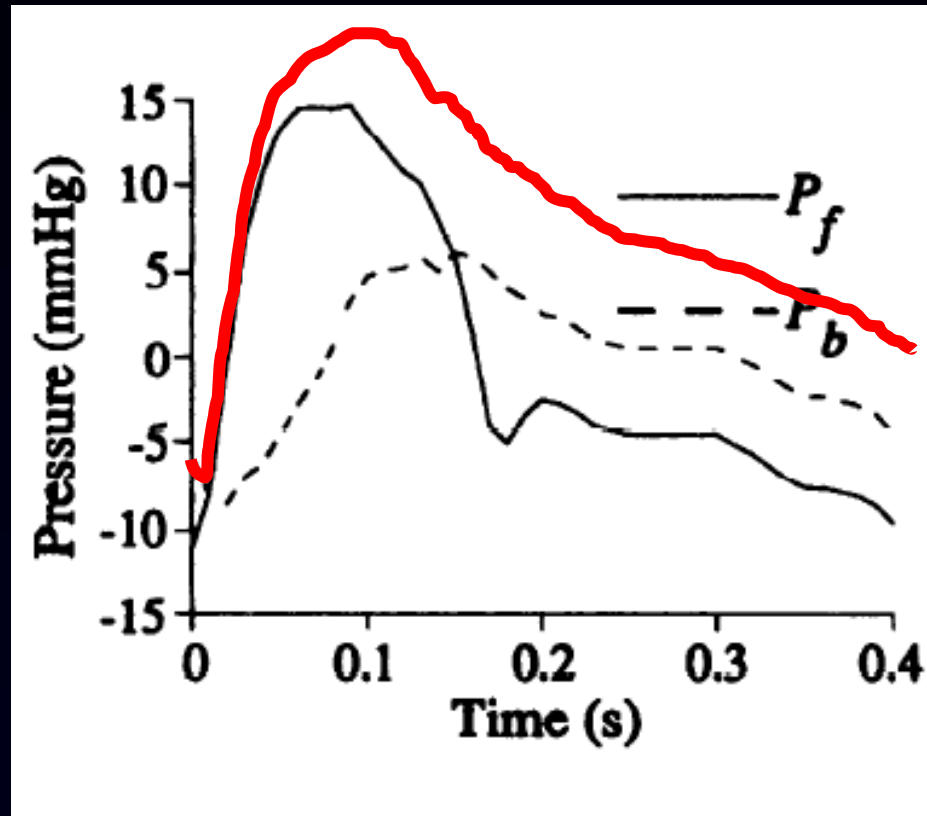


Les ondes de réflexion

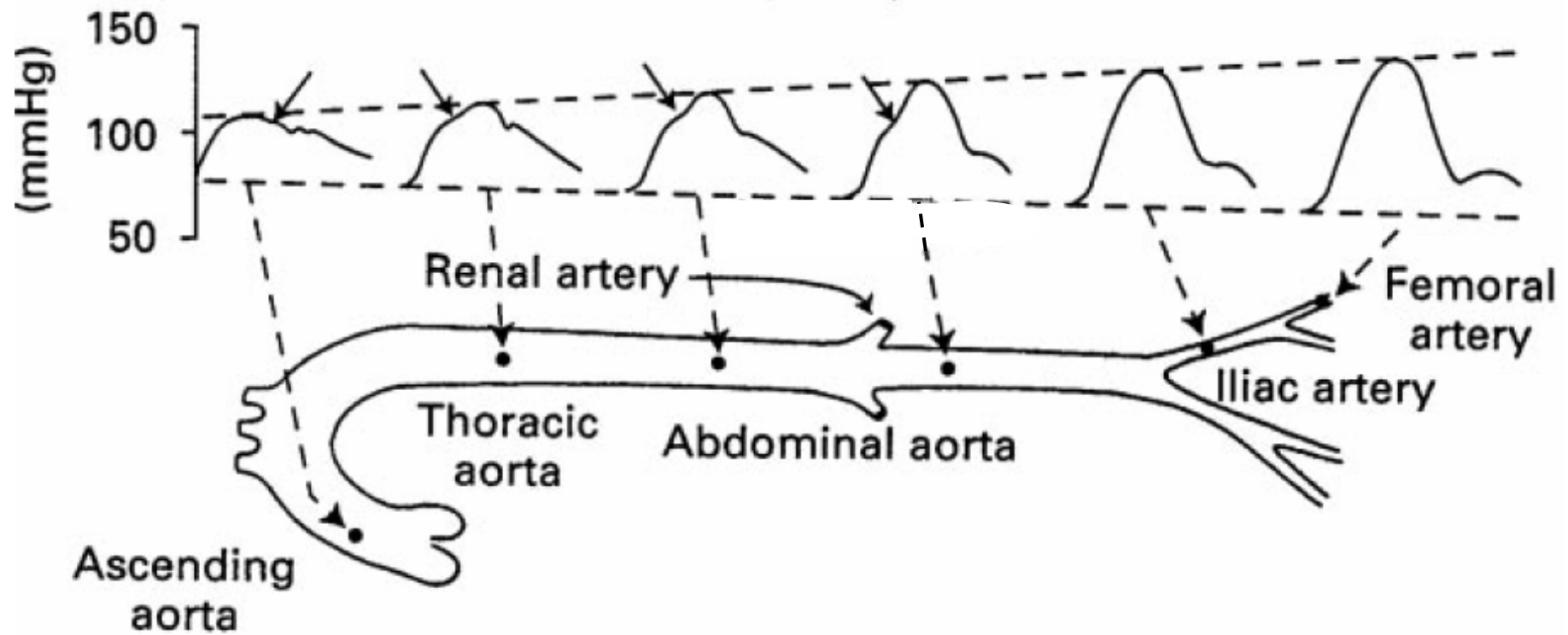
L'onde de pression artérielle se réfléchit chaque fois qu'elle rencontre des zones de changement d'impédance (points de bifurcation)



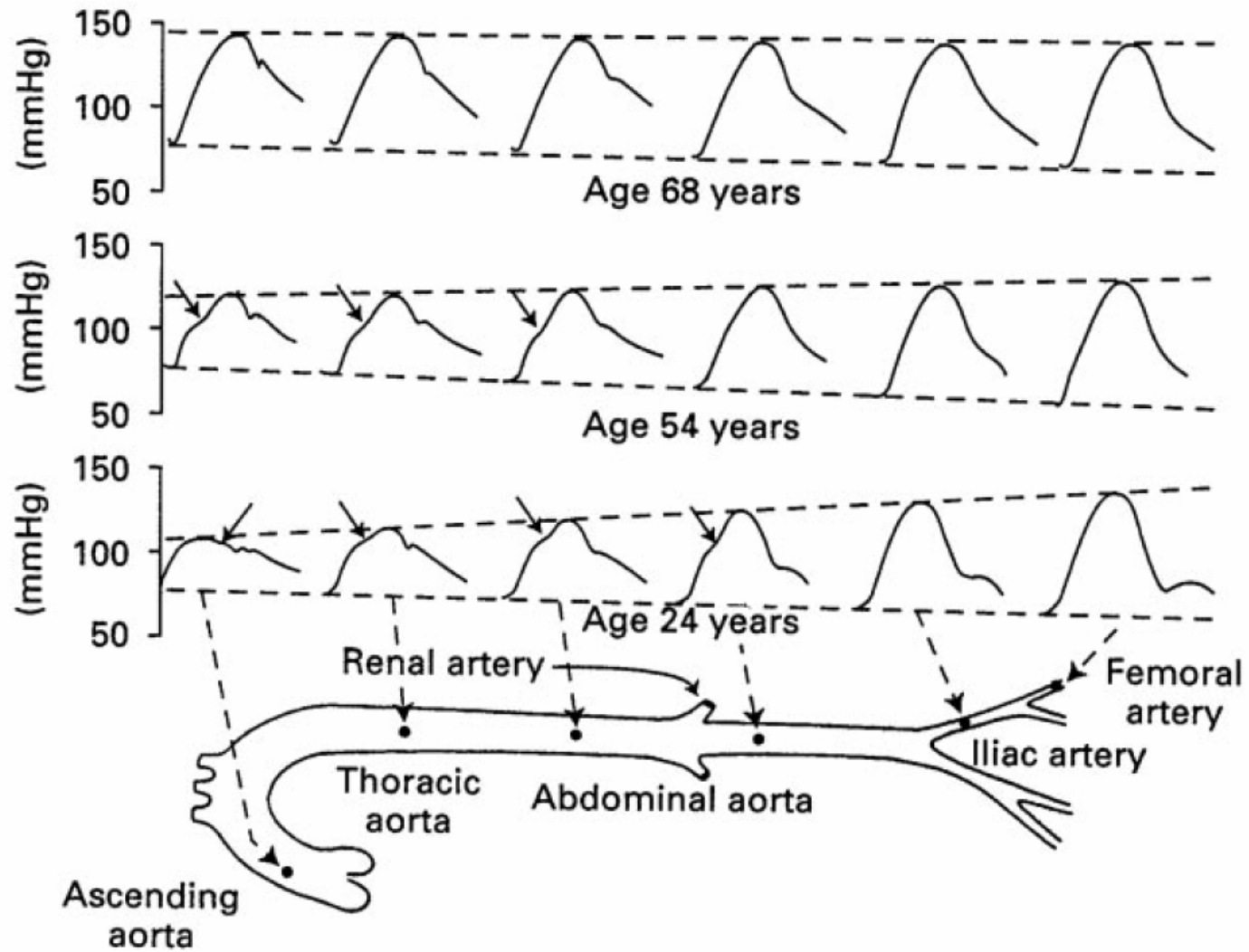
Les ondes de réflexion



Phénomène d'amplification de l'onde de pouls



Age and PP amplification



Pulse contour !

**Also takes into account waveform alteration due
to reflection waves**

Ejection volume derived from arterial pressure

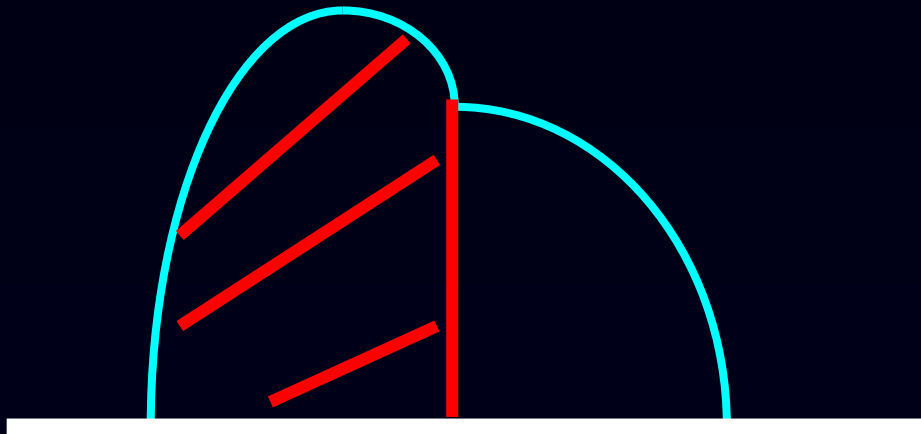
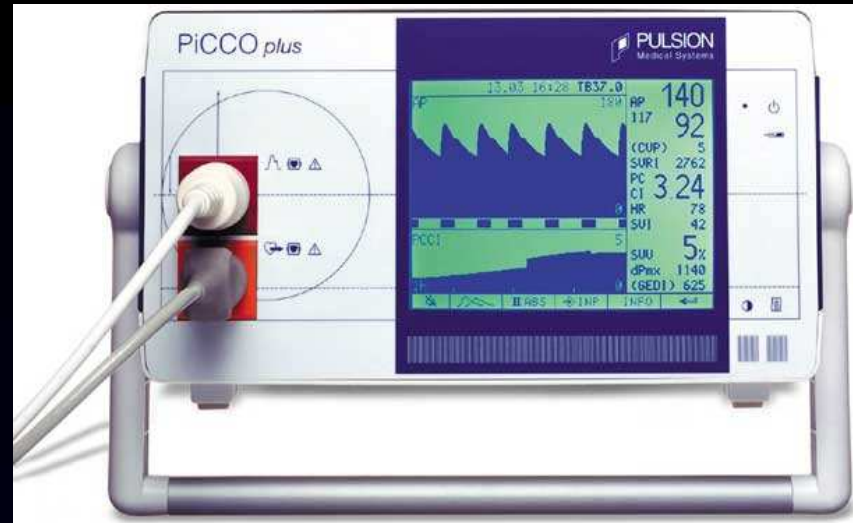
- PiCCO
- LiDCO
- APCO

Pulse contour is proportional to ejection volume, aortic elastance and vascular tone



=> calibration is mandatory for any change in vascular tone

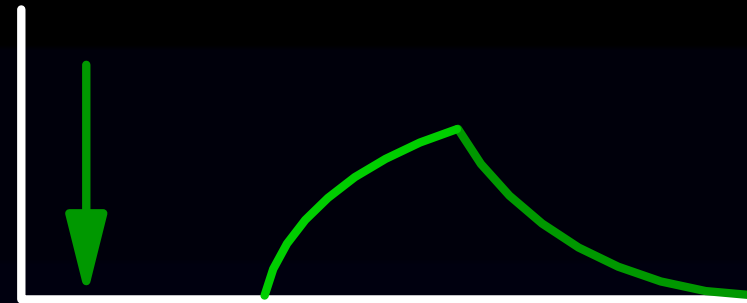
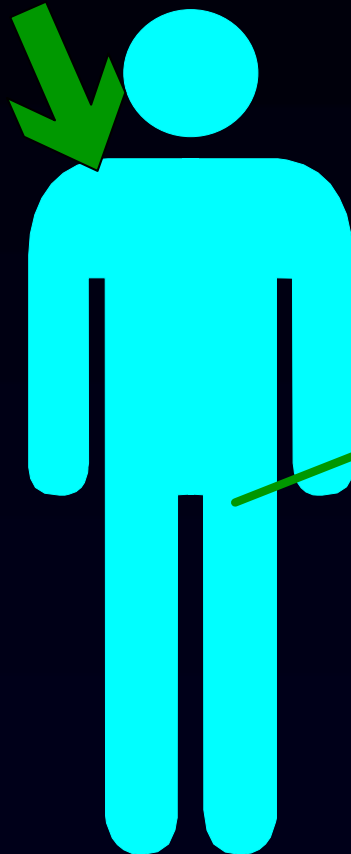
PiCCO



=> Importance of recognition of aortic dirotic wave

COLD / PICCO

IV injection of
cold ICG or saline

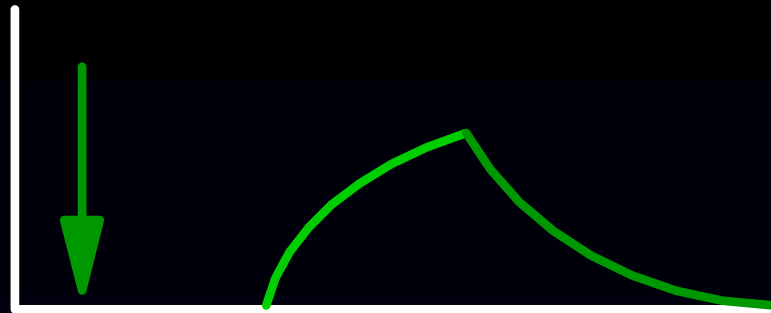
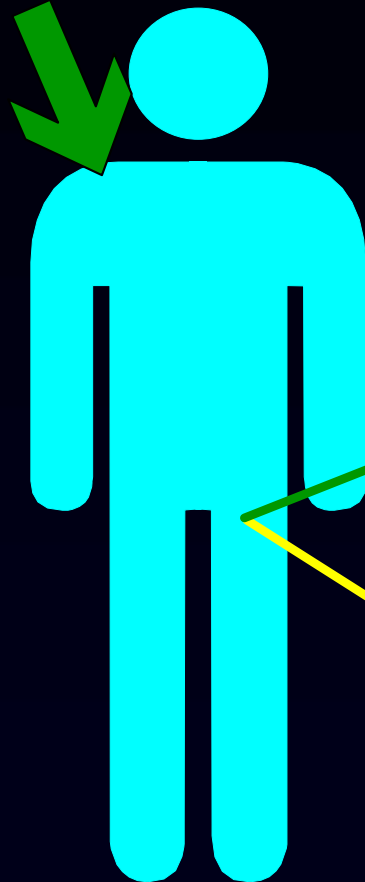


Transit time

thermodilution curve area

PICCO

IV injection of
cold saline



Transit time

thermodilution

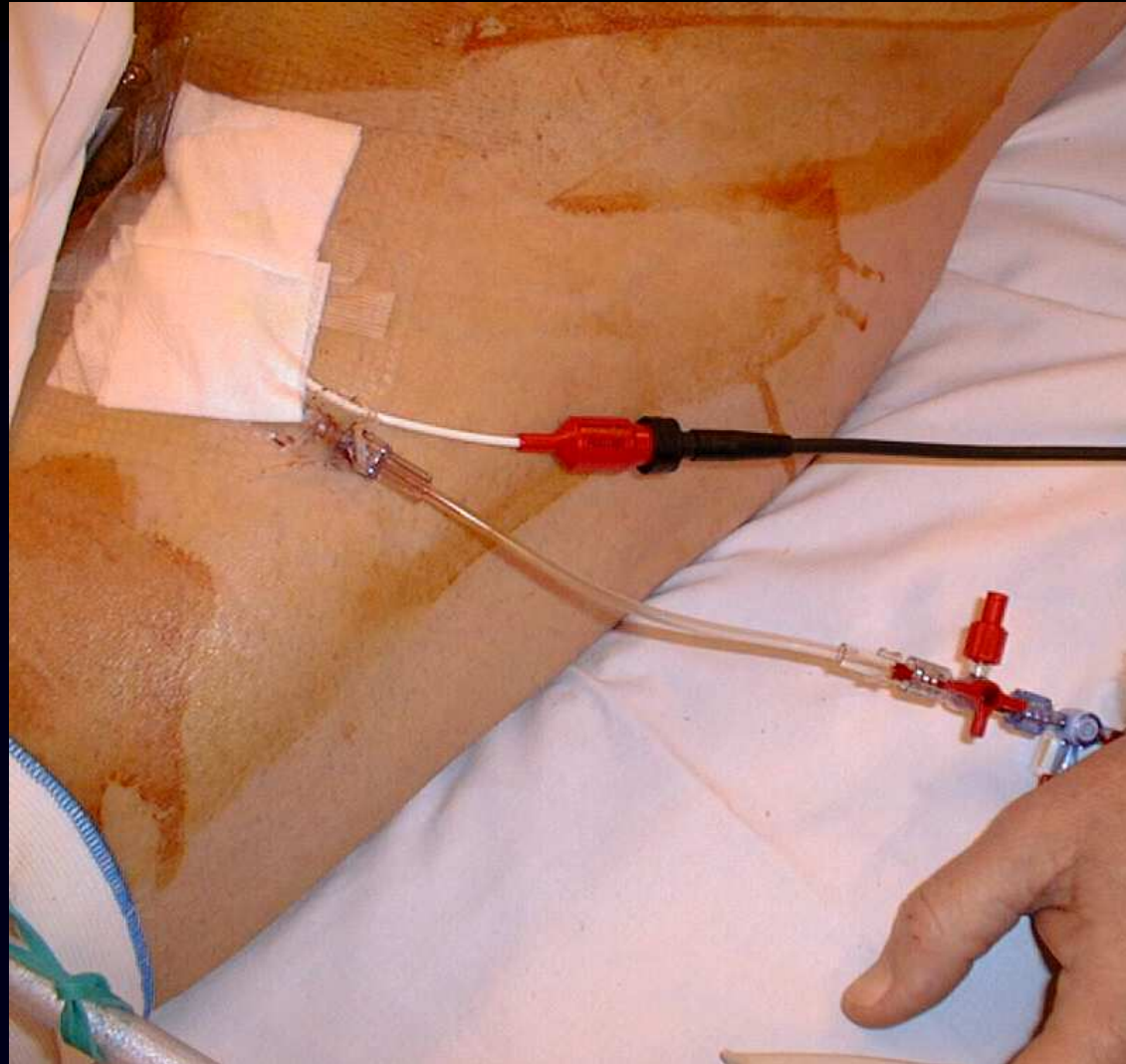
calibration

pressure contour analysis



DDB USI

PiCCO



PiCCO



PiCCO



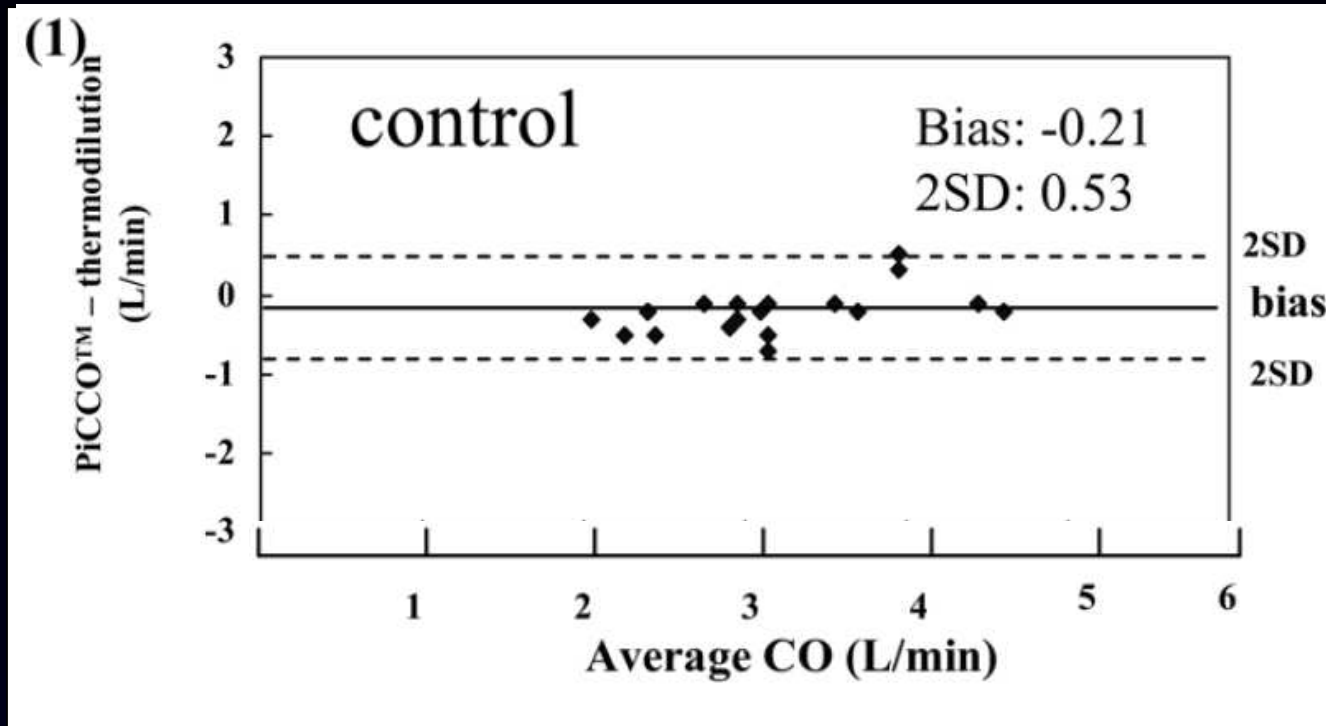
Advantages of PiCCO:

- Accurate measurements of CO (and DO₂)
- Additional data (GEDV, EVLW)
- Measurements of SVV

Disadvantages of PiCCO:

- Combines the errors of calibration and pulse contour
- Good signal required
- Mathematical coupling of CO and derived measurements (GEDV)
- Specific arterial catheter required

PiCCO vs PAC



20 pts OPCAB

Button et al
BJA 99:329;2007

	PCO-ICO (litre min ⁻¹)	CCO-ICO (litre min ⁻¹)
Intraoperative		
T1	0.5 (1.5)	0.2 (1.7)
T2	0.4 (1.7)	0.2 (2.0)
T3	0.3 (3.0)	0.4 (2.5)
Postoperative		
T4	0.2 (3.8)	0.3 (3.7)
T5	0.2 (2.5)	0.4 (2.2)
T6	0.1 (3.1)	0.5 (2.2)

PiCCO vs PAC
N=31

Mean CO ~4.5 – 5.5 L/min

Impact of changes in SVR (>15%)

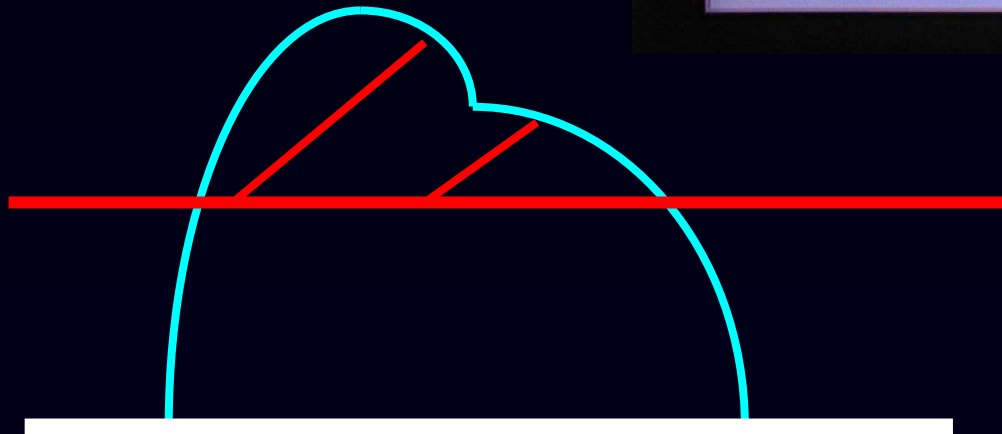
Hamzaoui et al
CCM 36:434;2008

Intervals of Time (Elapsed from the Previous Calibration)	n	r^2	p	Bias $\pm$ SD, L/min/m ²	Percentage Error
Within the first half hour	60	.79	<.001	0.04 $\pm$ 0.47	27
Between 30 mins and 1 hr	72	.74	<.001	0.07 $\pm$ 0.46	26
Between 1 and 2 hrs	66	.72	<.001	0.09 $\pm$ 0.58	32
Between 2 and 3 hrs	59	.65	<.001	0.16 $\pm$ 0.66	37
Between 3 and 4 hrs	45	.65	<.001	0.03 $\pm$ 0.63	35
Between 4 and 5 hrs	47	.62	<.001	0.14 $\pm$ 0.63	35
Between 5 and 6 hrs	51	.62	<.001	0.13 $\pm$ 0.66	36

PiCCO

N=59

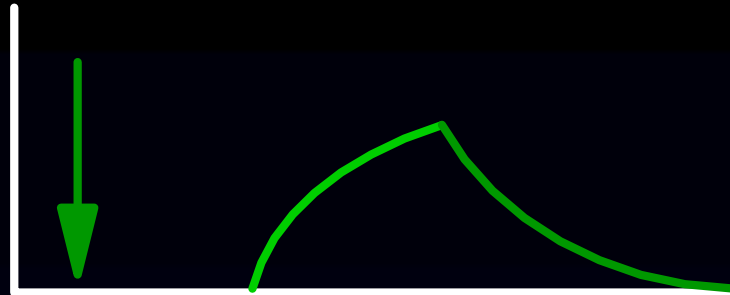
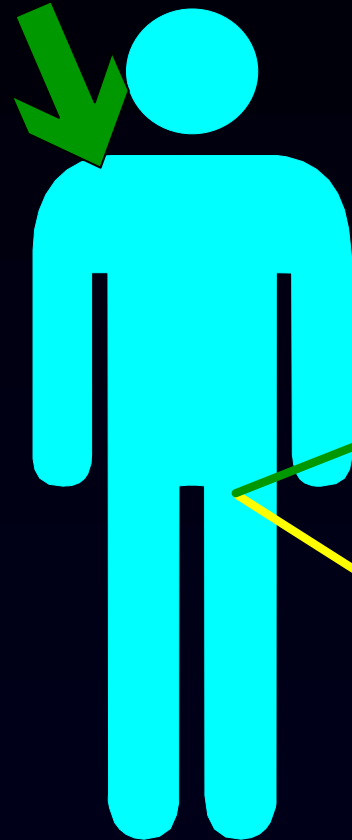
LiDCO



=> Recognition of aortic dicrotic wave less important

LiDCO

IV injection of
Lithium



Lithium dilution

calibration

pressure contour analysis



DDB USI

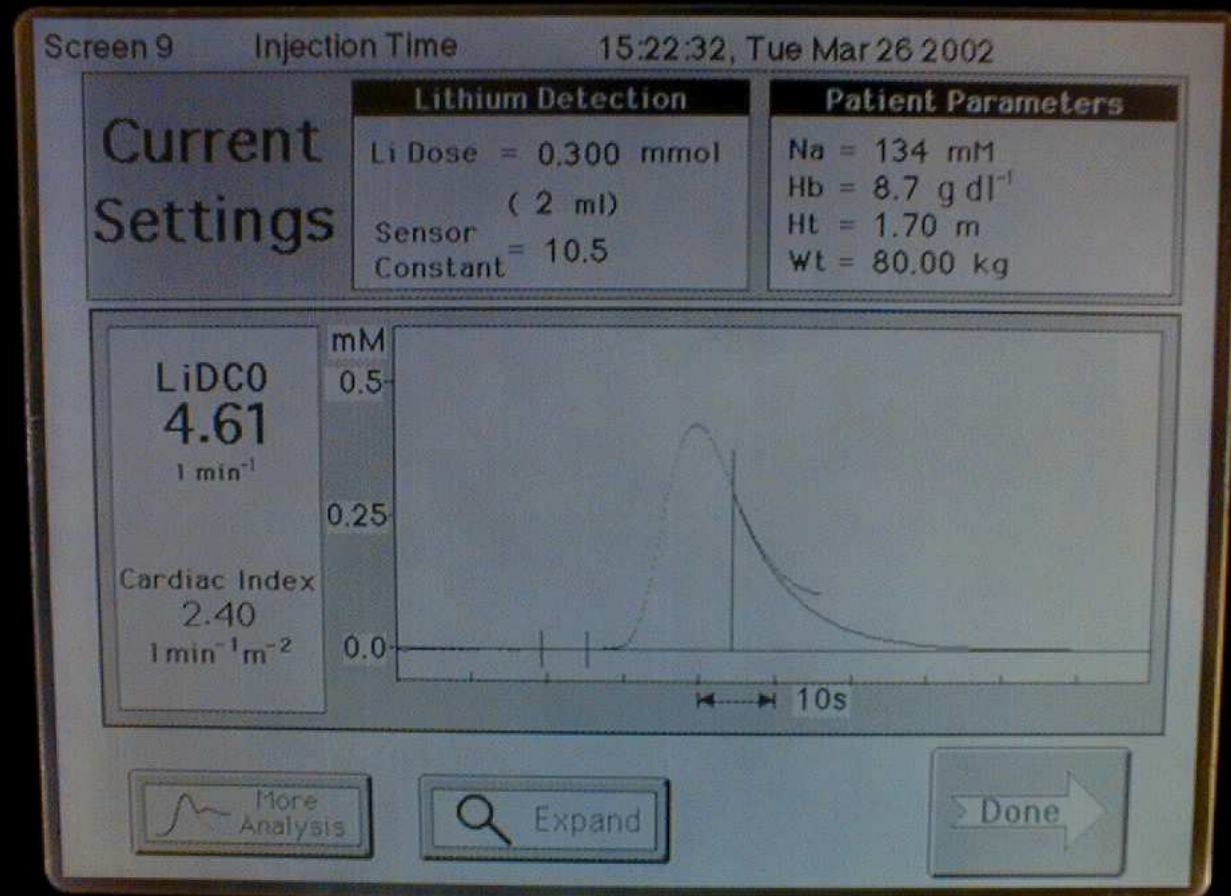
LiDCO



LiDCO



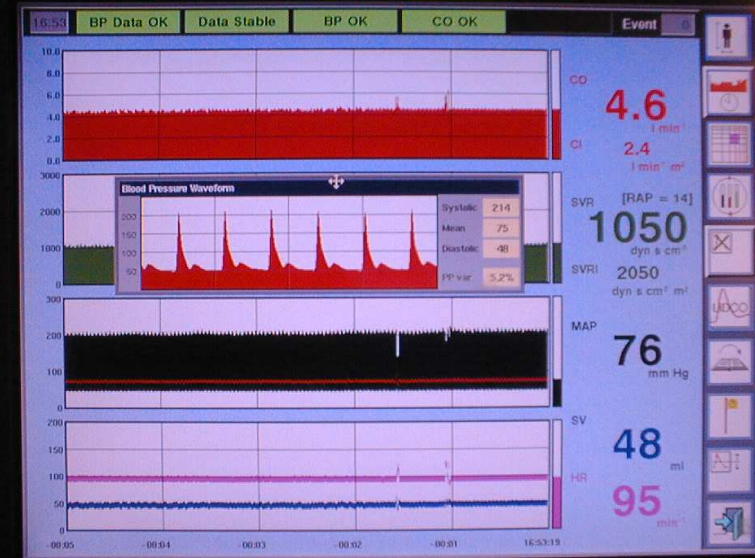
LiDCO



LiDCO



LiDCO



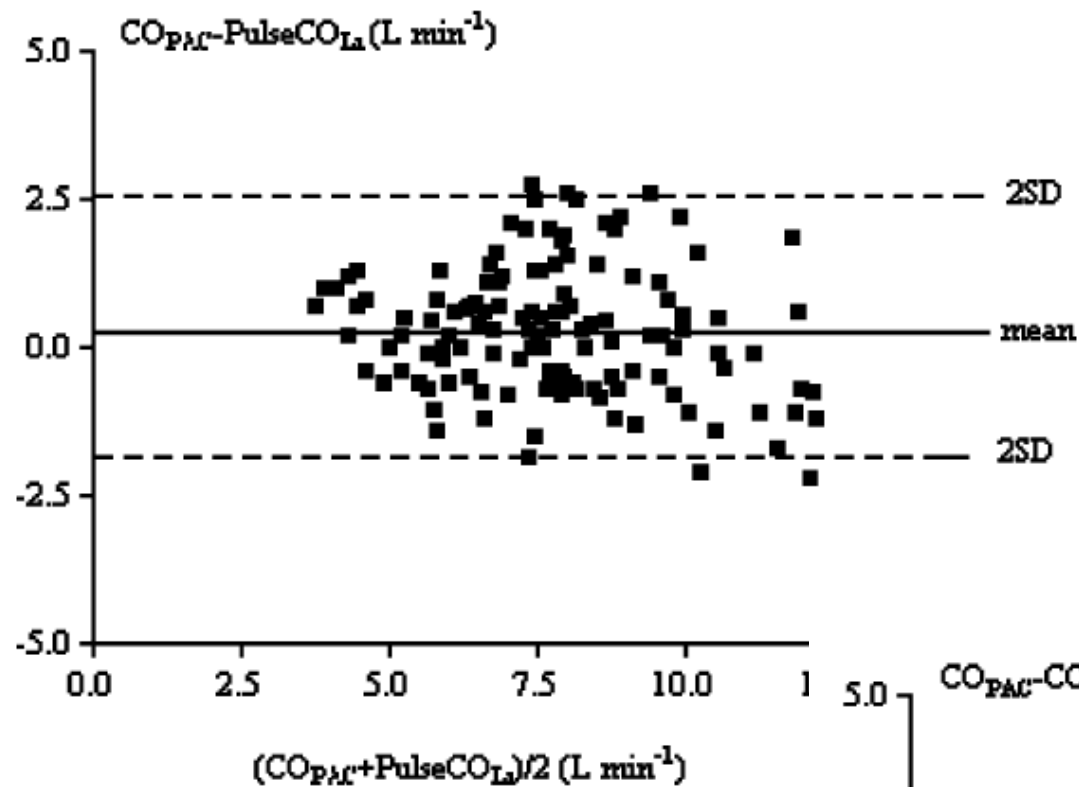
Advantages of LiDCO:

- Accurate measurements of CO (and DO₂)
- Calibration with Li more reliable than thermodilution
- Robust algorithm
- Measurements of SVV

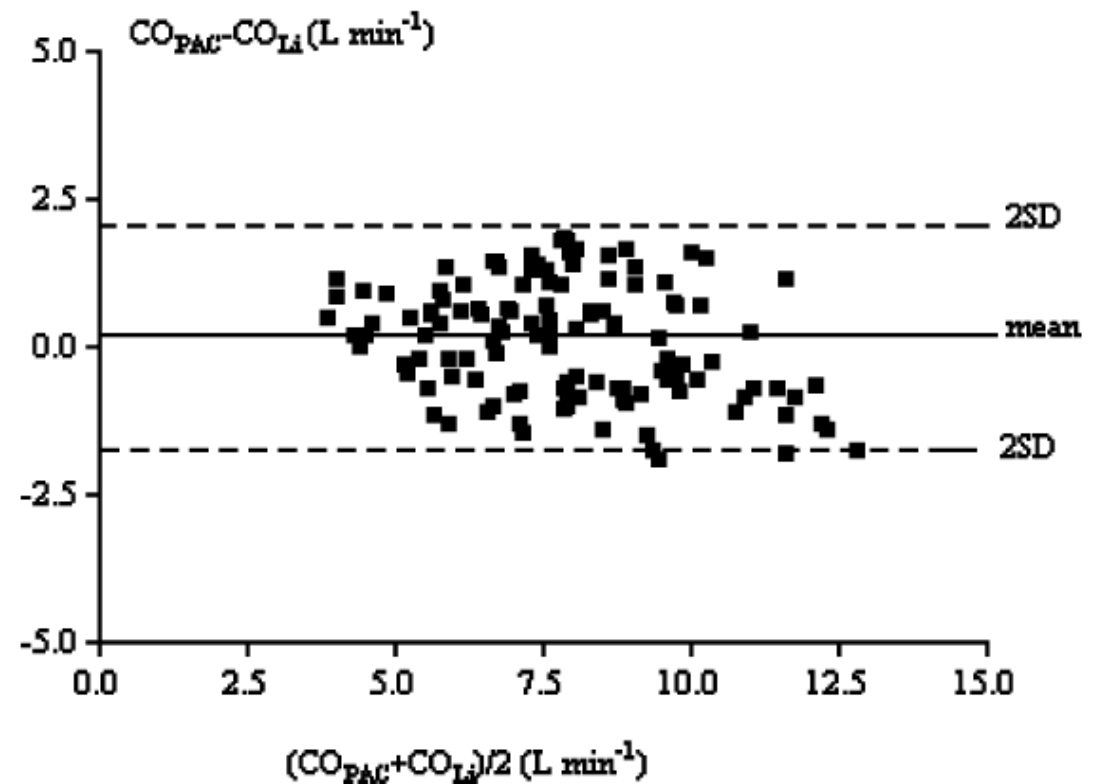
Disadvantages of LiDCO:

- Li can not always be used (=> calibration with other techniques?)
- Costs
- No other information than CO

Cecconi et al
ICM 34:257;2008



LiDCO vs PAC
Liver Tx N=23

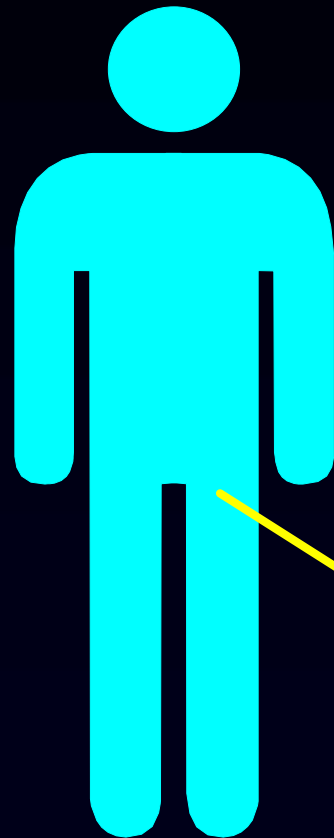


Level of CO	Observation	Bias (l min ⁻¹)	95% Limit of agreement	PE (%)
< 8 l min ⁻¹				
CO _{PAC} -CO _{Li}	78	0.08±1.61	-1.53 to 1.69	15.7
CO _{PAC} -PulseCO _{Li}	78	0.10±1.54	-1.44 to 1.64	15.1
CO _{Li} -PulseCO _{Li}	78	-0.06±1.19	-1.25 to 1.13	10.5
CO _{PAC} -CCO	78	0.52±2.37	-2.89 to 1.84	18.7
> 8 l min ⁻¹				
CO _{PAC} -CO _{Li}	73	0.14±2.25	-2.09 to 2.36	15.5
CO _{PAC} -PulseCO _{Li}	73	0.49±2.62	-2.13 to 3.11	18.5
CO _{Li} -PulseCO _{Li}	73	0.21±1.61	-1.40 to 1.82	9.24
CO _{PAC} -CCO	73	-0.44±2.71	-3.15 to 2.28	14.5

LiDCO vs PAC
Liver Tx N=23

APCO/Florac (Vigileo)

No calibration but
calculation of aortic
elastance form biometric
values and evaluation of
vascular tone by pulse
pressure



pressure contour analysis



Human database (AP curves and CO measurements using the reference iCO-PAC technique) in different clinical conditions

Biometric variables (age, gender)



$$\text{CO} = \text{pulse rate} \cdot \text{AP}_{\text{sd}} \cdot \chi$$



Shape variables

FloTrac 1st generation

G1

$$CO = \text{pulse rate} \cdot AP_{sd} \cdot \chi$$



**Updated every 10'
(shape variables)**

FloTrac 2nd generation

G2

$$CO = \text{pulse rate} \cdot AP_{sd} \cdot \chi$$



**Updated every 1'
(shape variables)**

FloTrac (APCO) G1

McGee et al
Crit Care 11:R105;2007

84 patients (69 surgical) from four ICUs. Average age was 68 (24-80) years, and 65% of the patients were male.

Range of cardiac output: 1.7 – 9.2 L/min (mean 6)

Grouped measurements (561 data points) for APCO, ICO and CCO were analyzed for bias, precision and correlation via Bland–Altman analysis.

Flowtrach (APCO)

McGee et al
Crit Care 11:R105;2007

APCO – ICO: Bias 0.2 L/M²

Limits of agreement +/- 2.6 L/min.M²

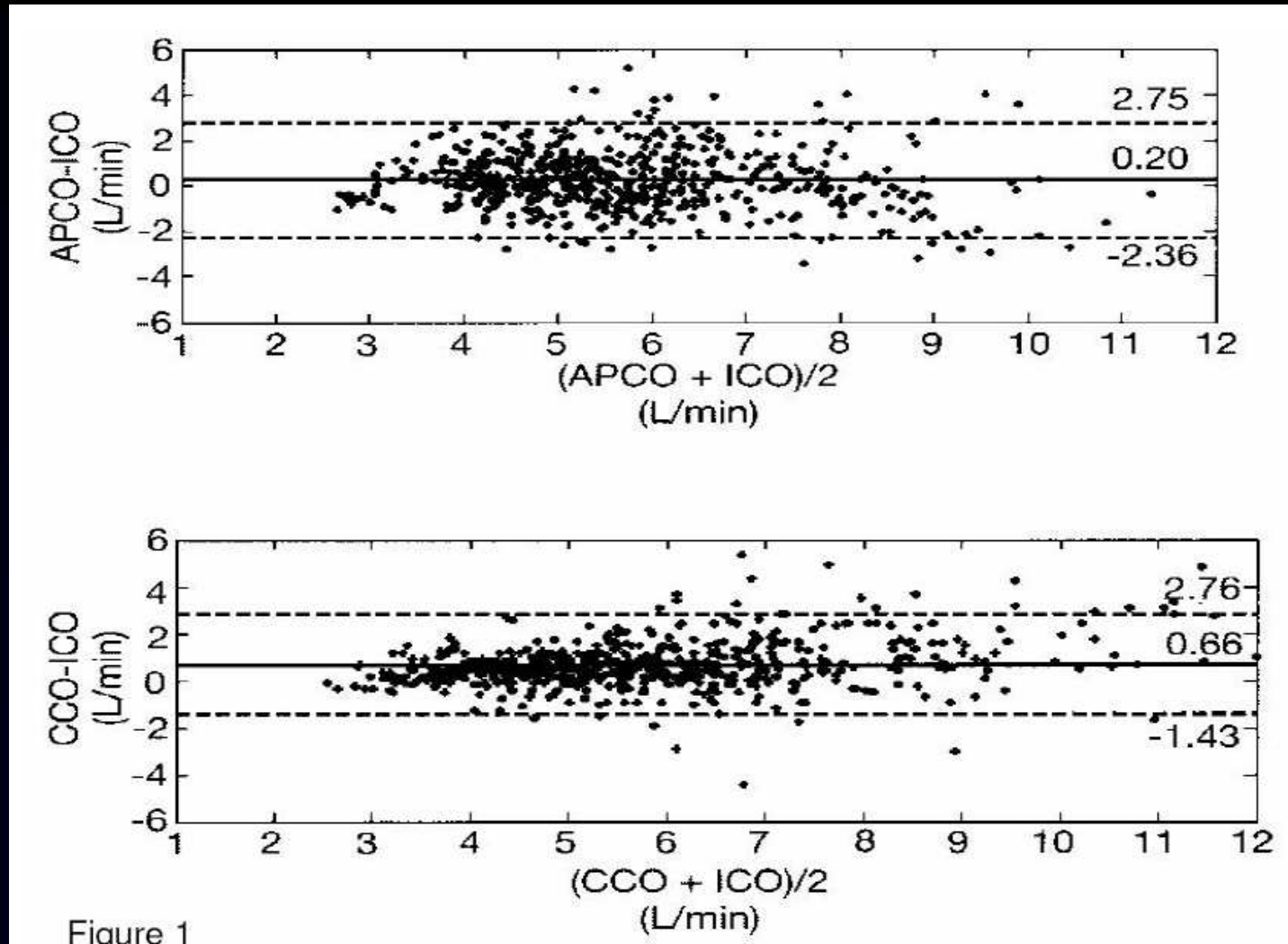
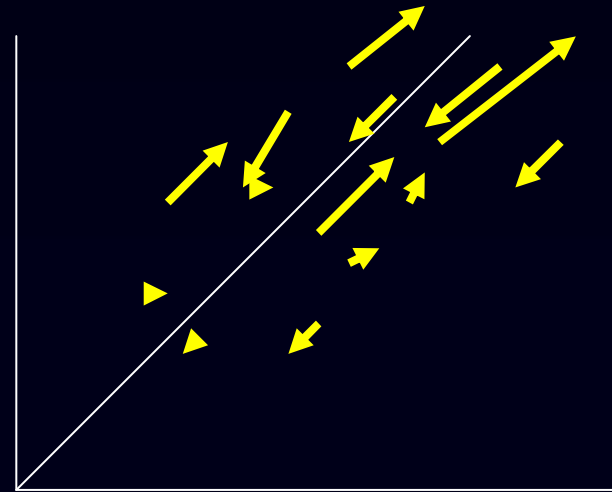
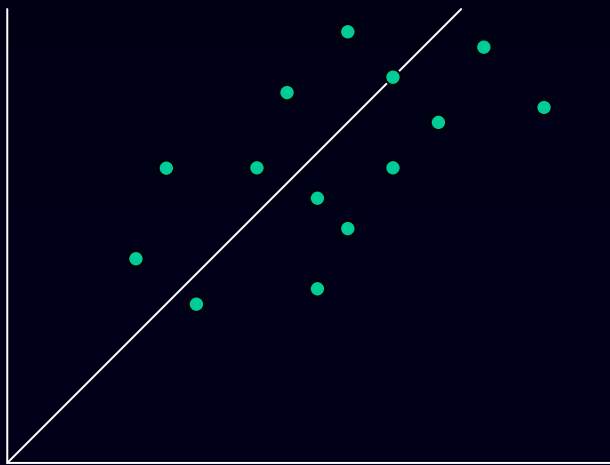


Figure 1

CCO – ICO: Bias 0.7 L/M²

Limits of agreement +/- 2.1 L/min.M²

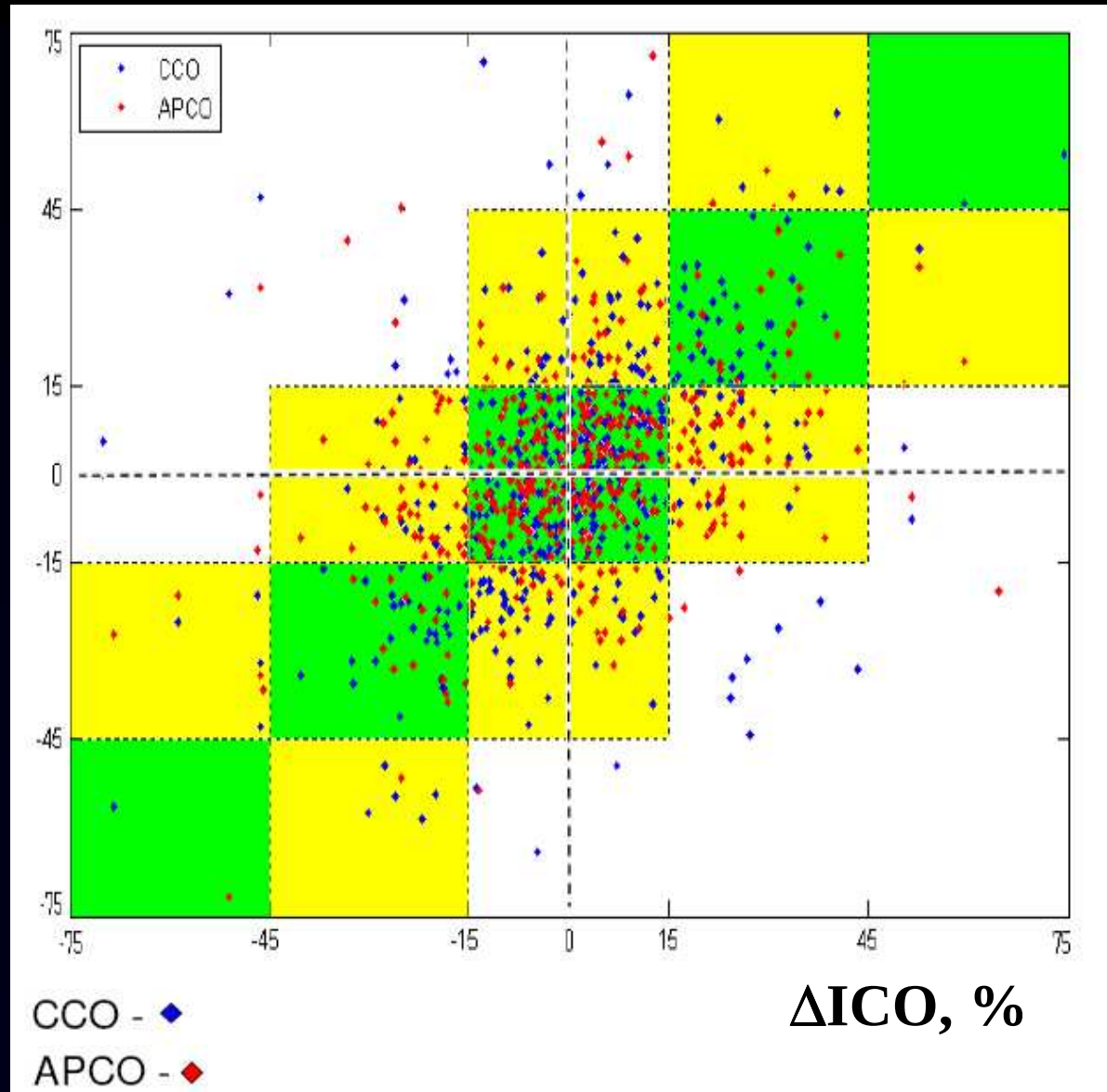
Precision of a given value of cardiac output is less important than reliability in trends.



Flowtrach (APCO)

McGee et al
Crit Care 11:R105;2007

%



Button et al
BJA 99:329;2007

	FCO-ICO (litre min ⁻¹)	PCO-ICO (litre min ⁻¹)	CCO-ICO (litre min ⁻¹)
Intraoperative period			
T1	0.6 (1.8)	0.5 (1.5)	0.2 (1.7)
T2	0.4 (1.9)	0.4 (1.7)	0.2 (2.0)
T3	0.1 (2.4)	0.3 (3.0)	0.4 (2.5)
Postoperative period			
T4	0.2 (2.5)	0.2 (3.8)	0.3 (3.7)
T5	0.1 (2.6)	0.2 (2.5)	0.4 (2.2)
T6	0.1 (2.4)	0.1 (3.1)	0.5 (2.2)

FloTrac vs PiCCO vs PAC
N=31

Mean CO ~4.5 – 5.5 L/min

Author	Year	Patients	Software	2sd/mean
deWaal and colleagues	2007	CABG	V 1.01	33%
Mayer and colleagues	2007	Cardiac	V 1.01	46%
Opdam and colleagues	2006	Cardiac	V 1.03	40%
Sander and colleagues	2006	CABG	V 1.03	54%
Manecke and Auger	2007	Cardiac	V 1.03	33%
Prasser and colleagues	2007	Neuro-ICU	V 1.03	49%
McGee and colleagues	2007	Mixed	V 1.03	50%
Breukers and colleagues	2007	Cardiac	V 1.03	36%
Sakka and colleagues	2007	Septic	V 1.07	35%
Lorsomradee and colleagues	2007	Cardiac	V 1.07	29–56%
Button and colleagues	2007	Cardiac	V 1.07	40%
Cannesson and colleagues	2007	CABG	V 1.07	37%
Prasser and colleagues	2007	CABG	V 1.10	26.9%
Mayer and colleagues	2008	CABG	V 1.10	24.6%
Compton and colleagues	2008	Medical-ICU	V 1.07/V 1.10	51.7%

**Scheeren et al
BJA 101:279;2008**

Time response (min)

	Time		
	PAC-CCO	NICOM™	Vigileo™
Negative	7.0 ± 2.6	1.3 ± 0.5*	1.1 ± 0.3*
Positive	9.4 ± 4.9	1.4 ± 0.5*	1.1 ± 0.3*
* $P < 0.05$			

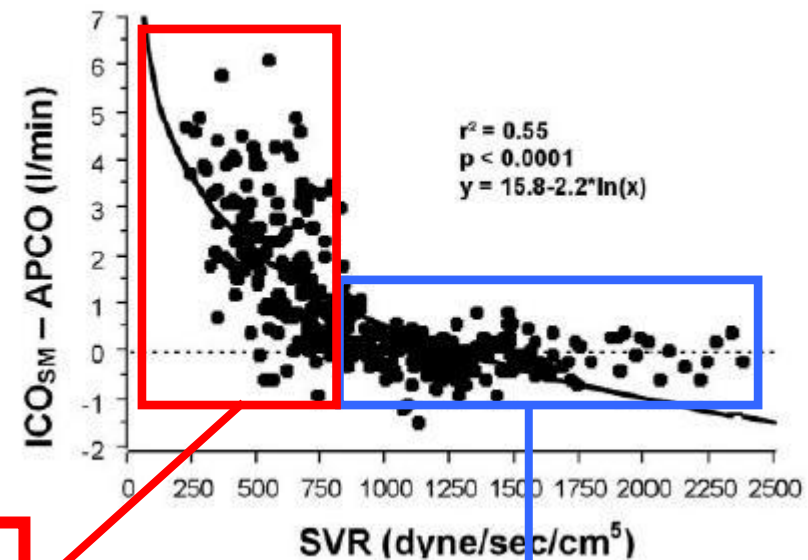
FloTrac 2nd generation (G2): good results in cardiac surgical patients

However, concerns have been raised in vasoplegic states (septic shock & liver transplantation) where FloTrac G2 may underestimate cardiac output

Cardiac Output Measurement in Patients Undergoing Liver Transplantation: Pulmonary Artery Catheter Versus Uncalibrated Arterial Pressure Waveform Analysis

Biais Matthieu, MD
Nouette-Gaulain Karine, MD, PhD
Cottenceau Vincent, MD
Vallet Alain, MD
Cochard Jean François, MD
Revel Philippe, MD
Sztark François, MD, PhD

CONCLUSIONS: Our results suggest that Vigileo/FloTrac CO monitoring data do not agree well with those of automatic thermodilution in patients undergoing liver transplantation, especially in Child-Pugh grade B and C patients with low systemic vascular resistance.
(Anesth Analg 2008;106:1480-6)



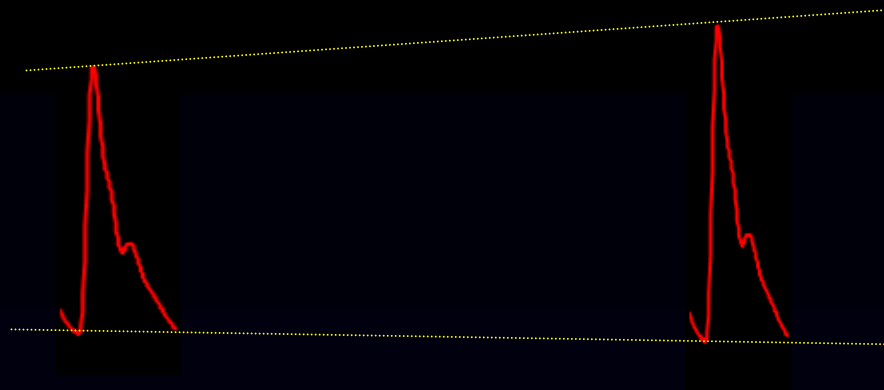
FloTrac underestimates Swan-Ganz cardiac output in low SVR patients (<800 dynes/sec/cm⁵)

FloTrac shows very good agreement in "normal to high" SVR patients (>800 dynes/sec/cm⁵)

Suspected mechanism?

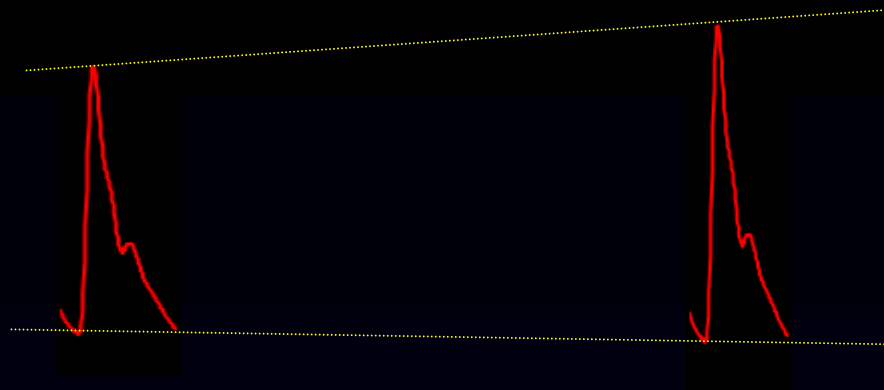
« Peripheral decoupling » ?

= gradient between central and peripheral arterial pressure



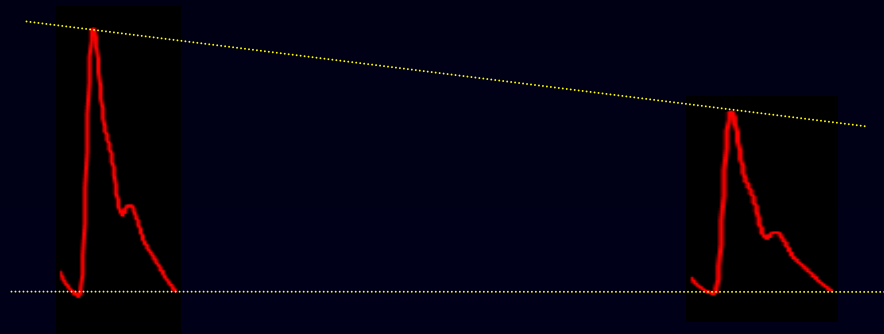
Normal state
Slight pulse amplification

Aorta  **Peripheral artery**

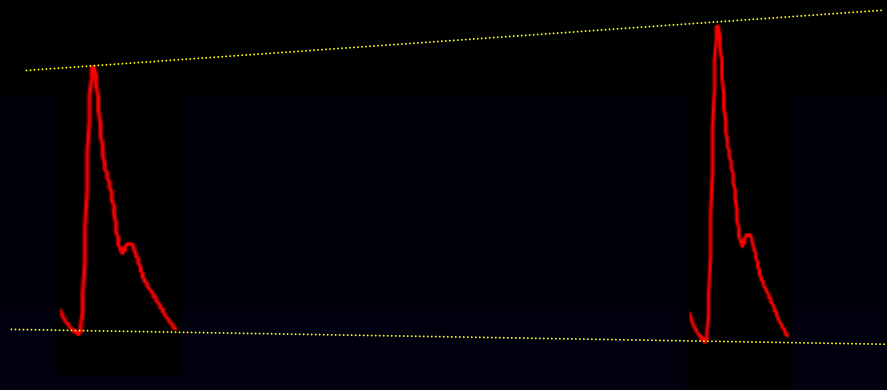


Normal state
Slight pulse amplification

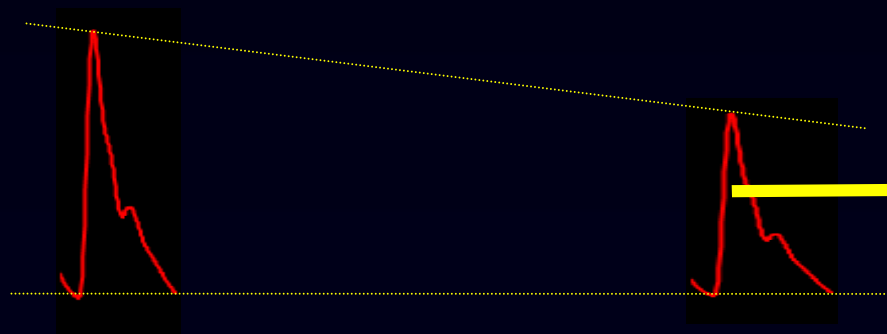
Aorta  **Peripheral artery**



Vasodilatory state
Significant pulse decrease

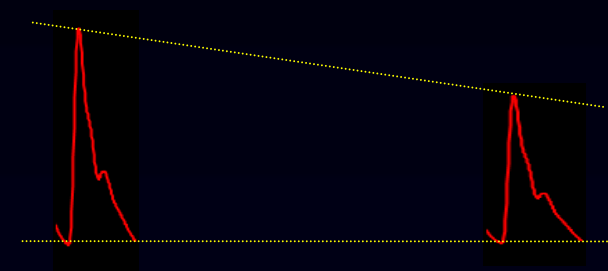
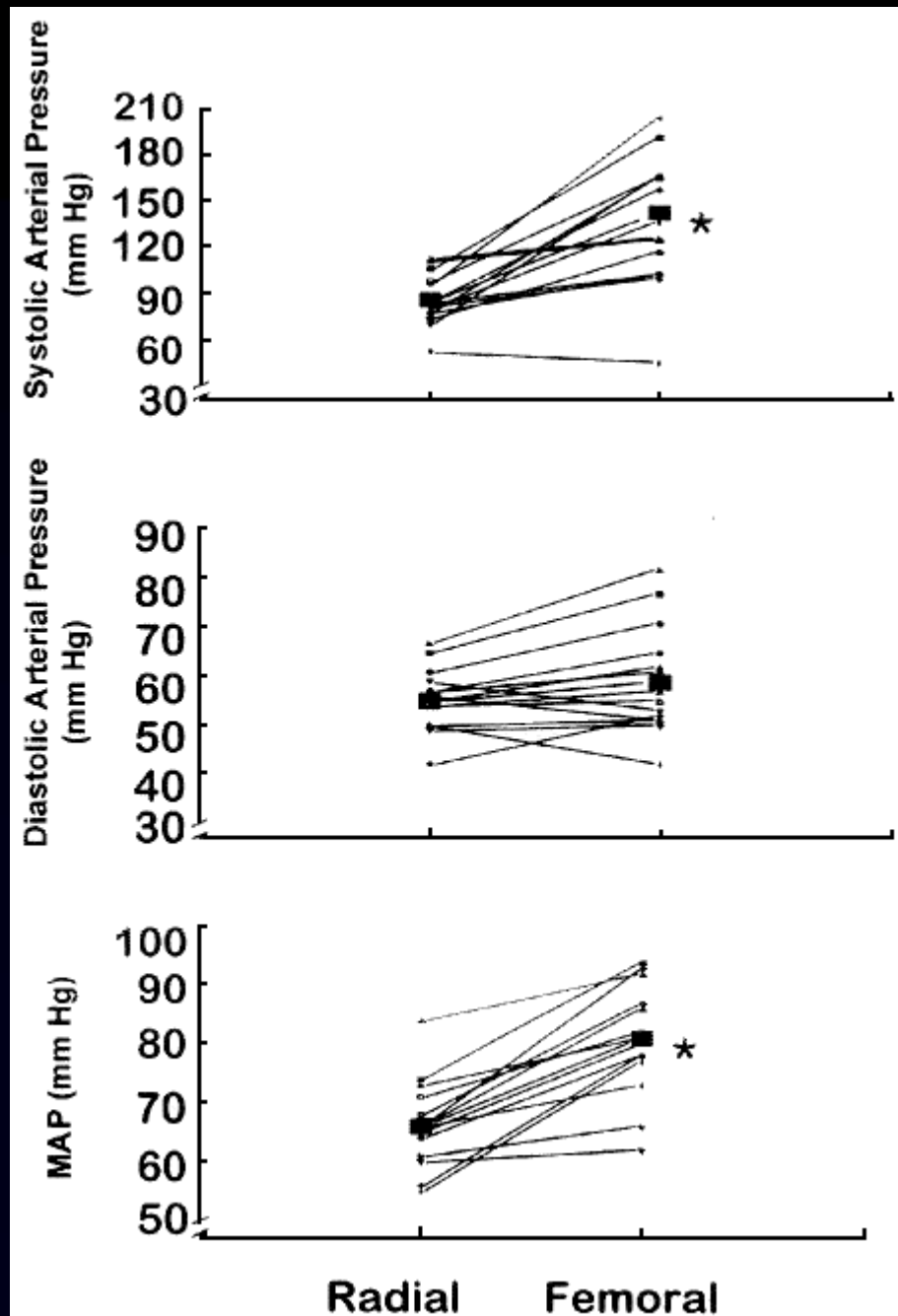


Aorta → Peripheral artery



Underestimation of SV

Dorman T et al
CCM 26:1646;1998

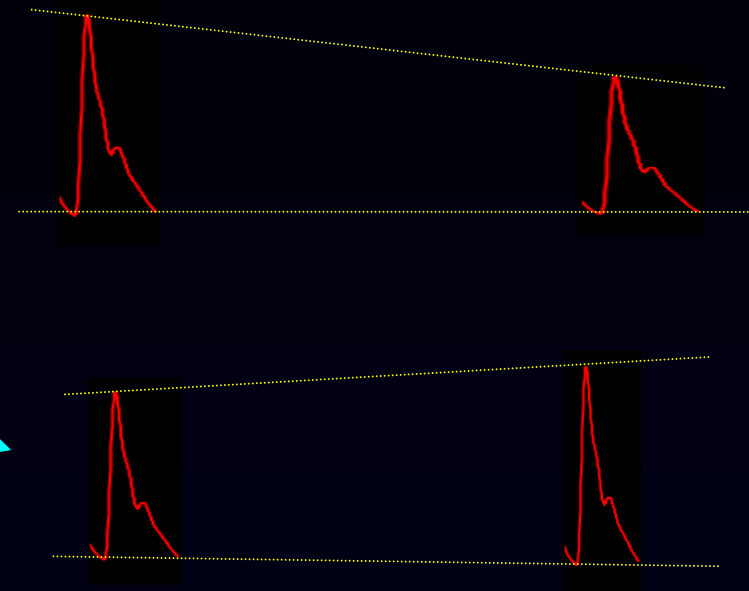


**14 pts with
septic shock**

	SBP (mm Hg)	DBP (mm Hg)	MAP (mm Hg)
On Norepinephrine			
Patient 1	-55	0	-15
Patient 2	-80	0	-18
Off Norepinephrine			
Patient 1	22	-19	0
Patient 2	21	-17	0

SBP, systolic blood pressure; DBP, diastolic blood pressure; MAP, mean arterial pressure.

This two-part table shows the radial to femoral pressure gradient from the two patients in whom simultaneous recordings were obtained while the patients received vasopressors, and after they were weaned from vasopressors. The gradients were calculated by subtracting the femoral pressure from the simultaneously recorded radial artery pressure.

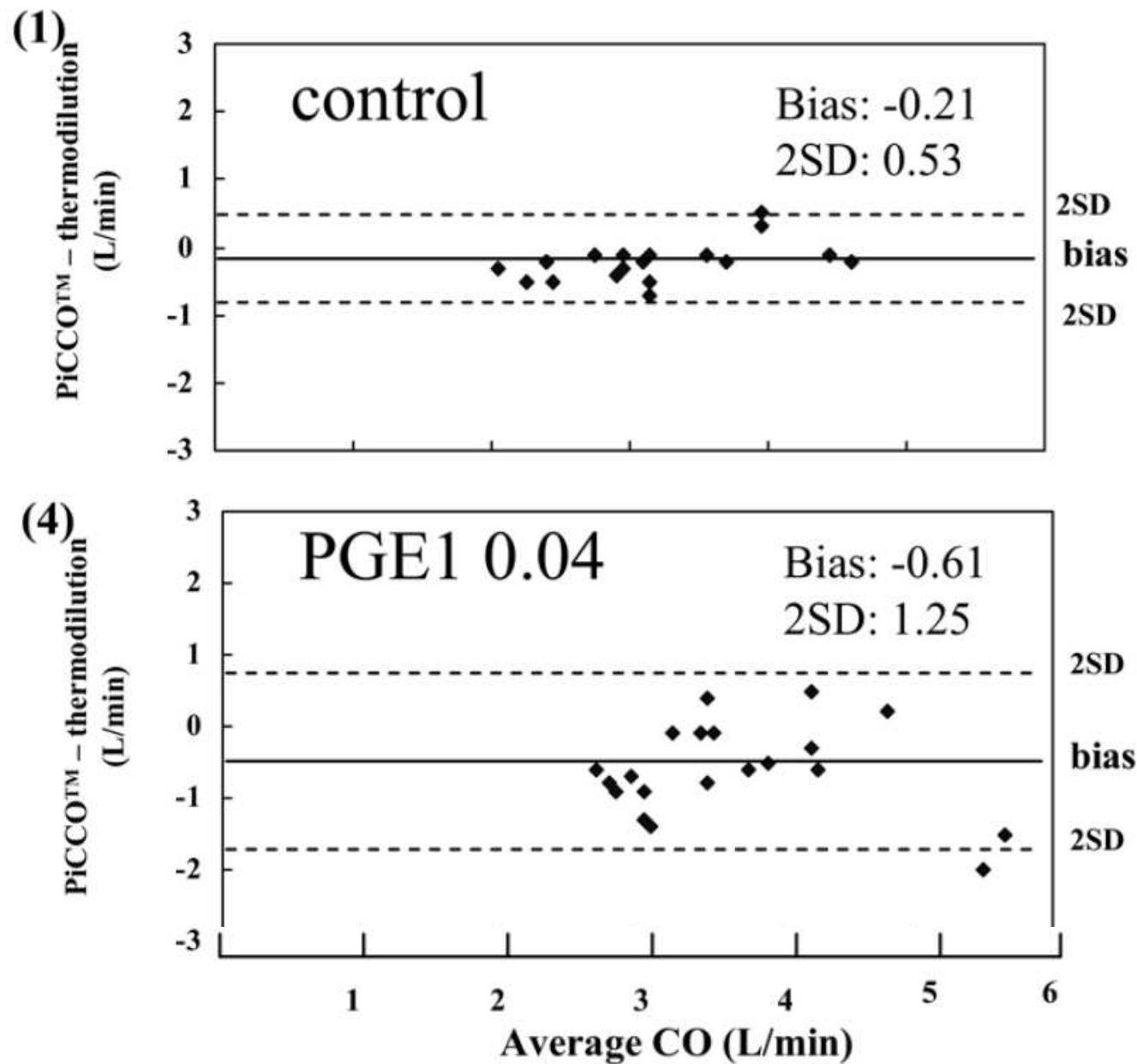


...also with other
pulse contour methods

Jellena et al
Anesthesiology 1999

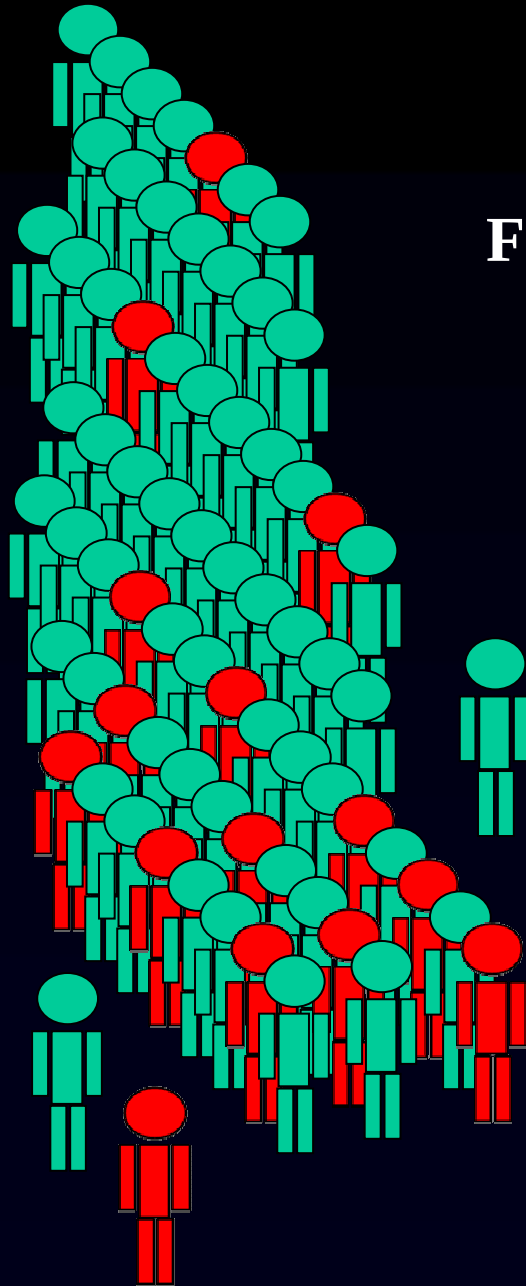
Precalibration Measurements of Day 1			
	Number	Bias (l/min)	95% Limits of Agreement
TDCO < 8	18	-0.86 ± 1.51	-3.81 to 2.10
TDCO ≥ 8	14	$-2.45 \pm 1.92^*$	-8.19 to 1.63
HR < 110	16	-1.88 ± 1.78	-5.4 to 1.6
HR ≥ 110	16	-1.96 ± 2.82	-7.5 to 3.6
MAP < 80	15	-2.06 ± 2.82	-7.58 to 3.46
MAP ≥ 80	17	-1.80 ± 1.85	-5.42 to 1.83
SVR < 800	15	-2.66 ± 2.79	-8.14 to 2.81
SVR ≥ 800	17	-1.26 ± 1.61	-4.4 to 1.90
Radial	25	-2.32 ± 2.35	-6.93 to 2.28
Femoral	7	-0.48 ± 1.59	-3.59 to 2.64

Postcalibration Measurements		
	Number	95% Limits of Agreement
	58	-0.05 ± 0.59 -1.21 to 1.10
	79	-0.15 ± 0.87 -1.86 to 1.56
	74	-0.02 ± 0.60 -1.19 to 1.14
	63	-0.21 ± 0.92 -2.01 to 1.59
	65	-0.05 ± 0.70 -1.42 to 1.32
	72	-0.16 ± 0.82 -1.77 to 1.42
	84	-0.17 ± 0.87 -1.87 to 1.53
	53	0.01 ± 0.54 -1.05 to 1.07
	108	-0.04 ± 0.74 -1.49 to 1.40
	29	-0.18 ± 0.73 -1.58 to 1.33



PiCCO vs PAC

20 pts OPCAB



FloTrac 3rd generation

G3

1. More patients in the human database
2. Higher proportion of vasoplegic states
3. More shape variables to calculate χ

$$CO = \text{pulse rate} \cdot AP_{sd} \cdot \chi$$

CO G3: Validation study

58 patients with sepsis *

401 cardiac output (CO) measurements

Pulmonary artery catheter to measure iCO and CCO
Reference CO = iCO

Radial (n=32) or femoral (n=26) arterial line
Arterial pressure recorded on a computer and
analyzed using CO_{G2} and CO_{G3}

*** Cohort independent from that used to develop the G3 algorithm**

CO G3: Validation study

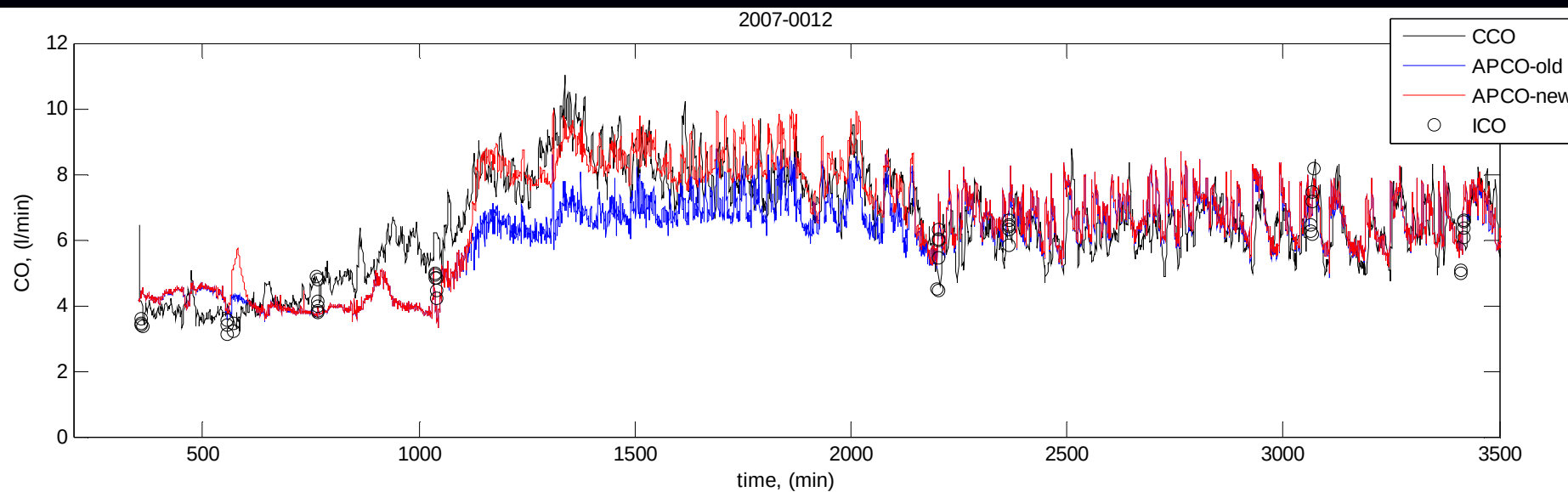
Methods:

- **ICO 3-5 boluses averaged***
- **CCO: 2 before and 3 after ICO boluses (~5min)**
- **CO G2/G3: averaged for 5 min (7 values before and 8 values after ICO measurement)**

*** ICO measurements: average values were included only when total variability of the 3-5 bolus was < 15%**

Hear rate (bpm)	97 ± 19
Mean arterial pressure (mmHg)	76 ± 11
iCO (l/min)	7.5 ± 2.0
CO_{G2} (l/min)	6.5 ± 1.5
CO_{G3} (l/min)	7.3 ± 2.1
CCO (l/min)	8.1 ± 2.1
SVR (dynes/sec/cm⁵)	875 ± 283

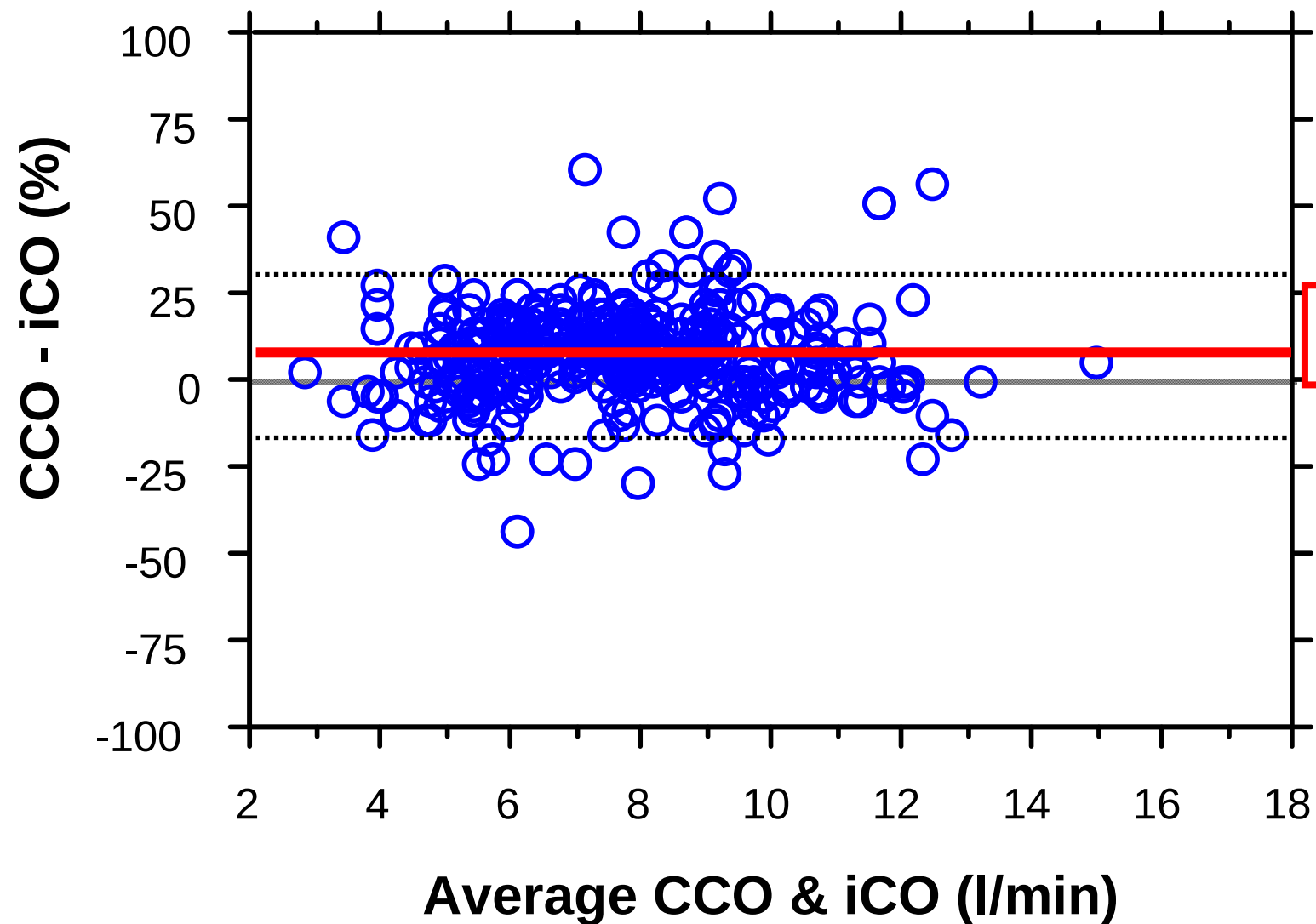
CO G3: Validation study



○ ICO from Swan-Ganz — CCO from Swan-Ganz — 2nd Generation — 3rd Generation

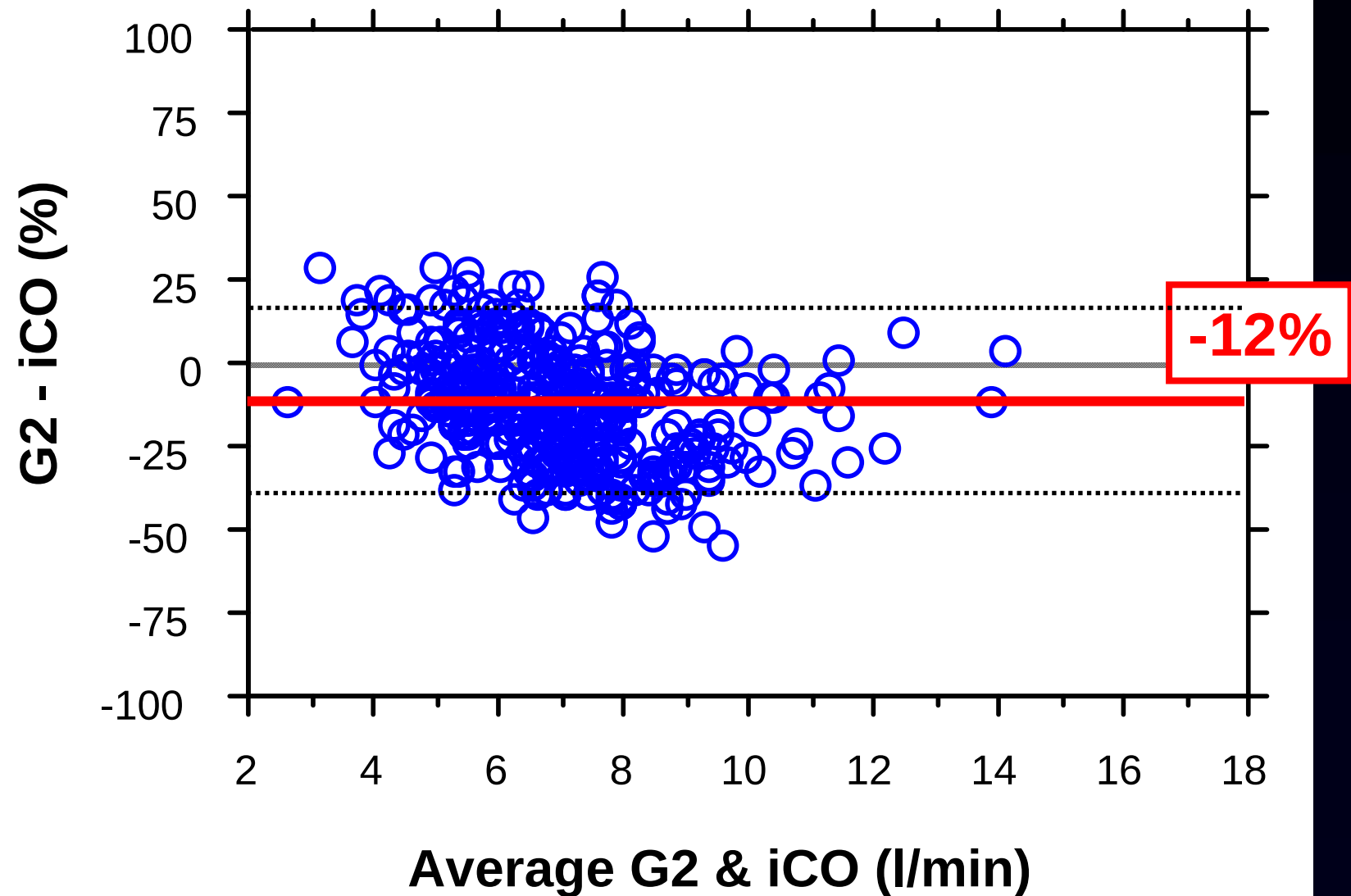
CCO

LOA 2.2 L/min



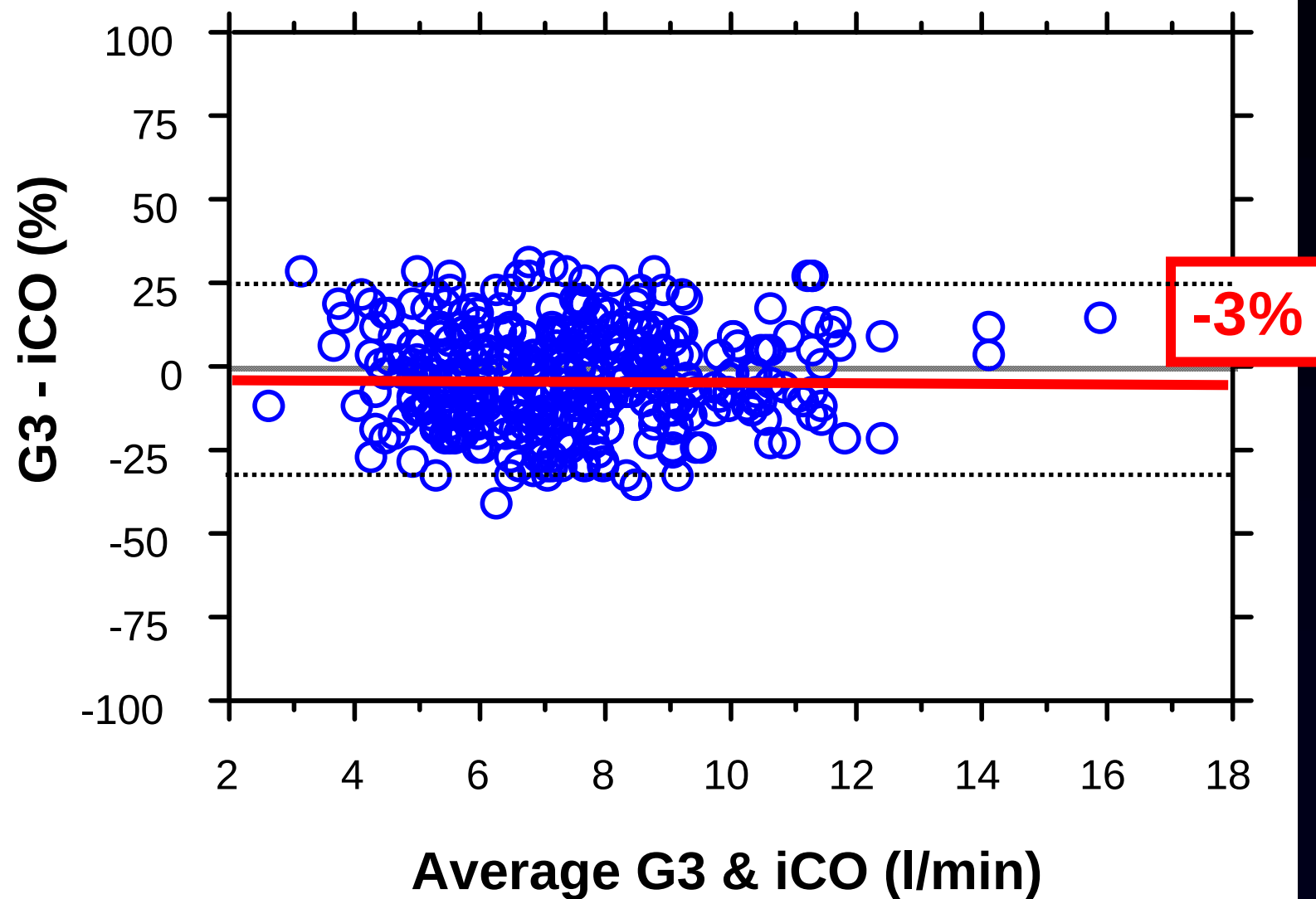
G2

LOA 2.4 L/min

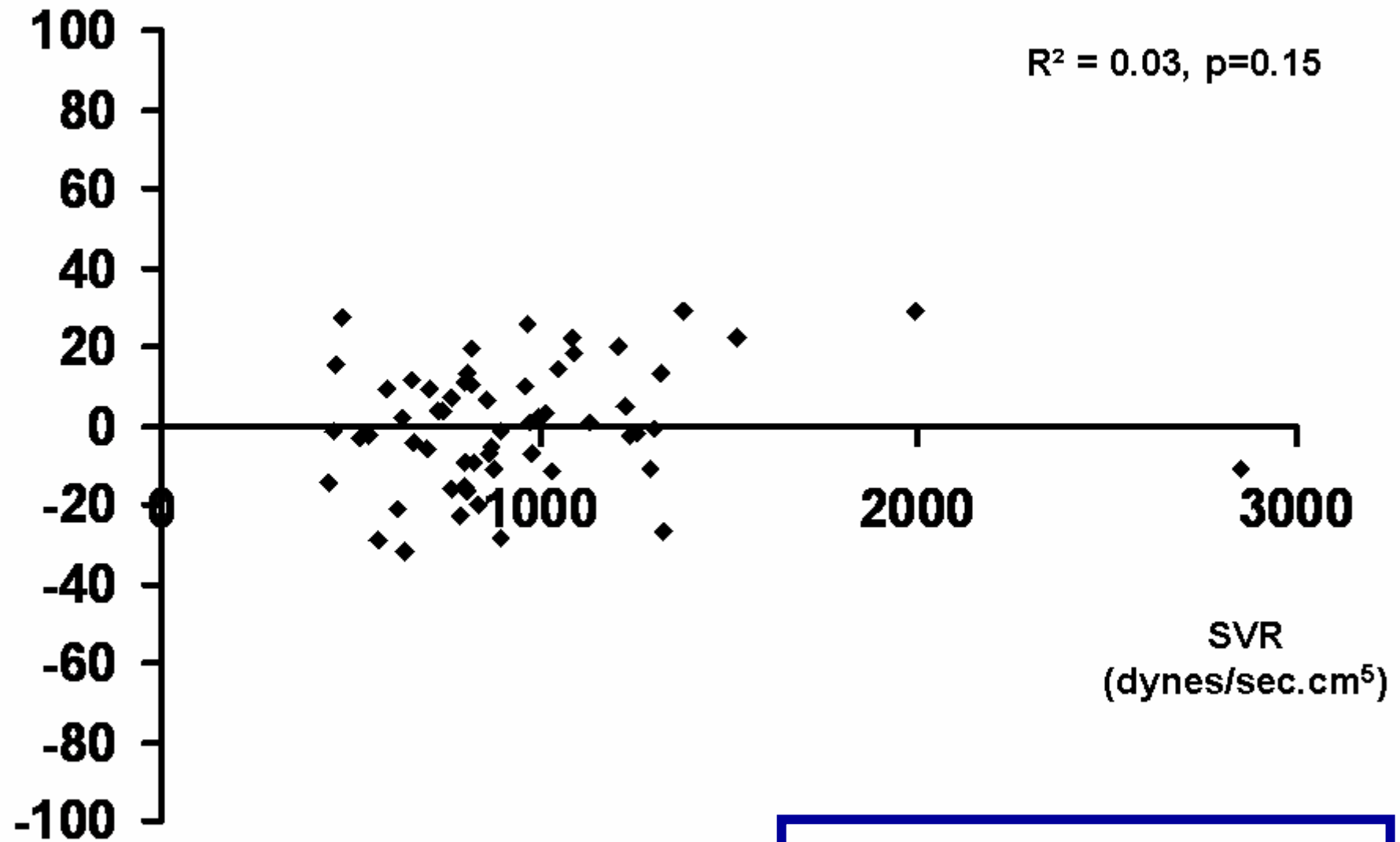


G3

LOA 2.2 L/min



$\text{CO}_{\text{G3}} - \text{iCO} (\%)$



Only one measurement /pt
(first one)

401 comparisons with iCO-PAC in 58 patients

G2

Bias (l/min) = -1.0
LOA (l/min) = 2.4
Bias (%) = -12 ± 16
%Error = 33%

G3

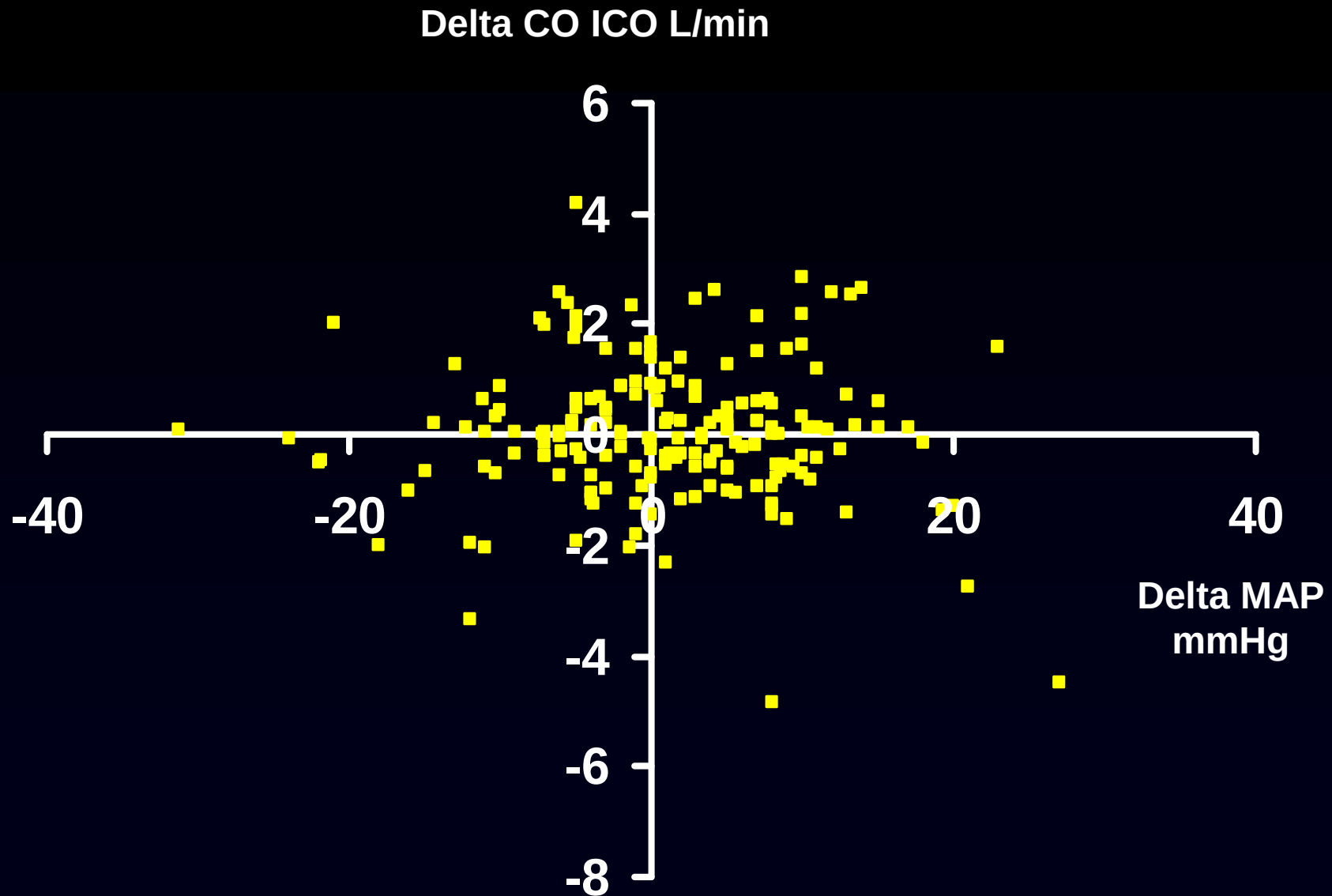
Bias (l/min) = -0.2
LOA (l/min) = 2.2
Bias (%) = -3 ± 15
%Error = 29%

CCO

Bias (l/min) = 0.6
LOA (l/min) = 2.2
Bias (%) = 8 ± 13
%Error = 29%

Detection of changes in CO ?

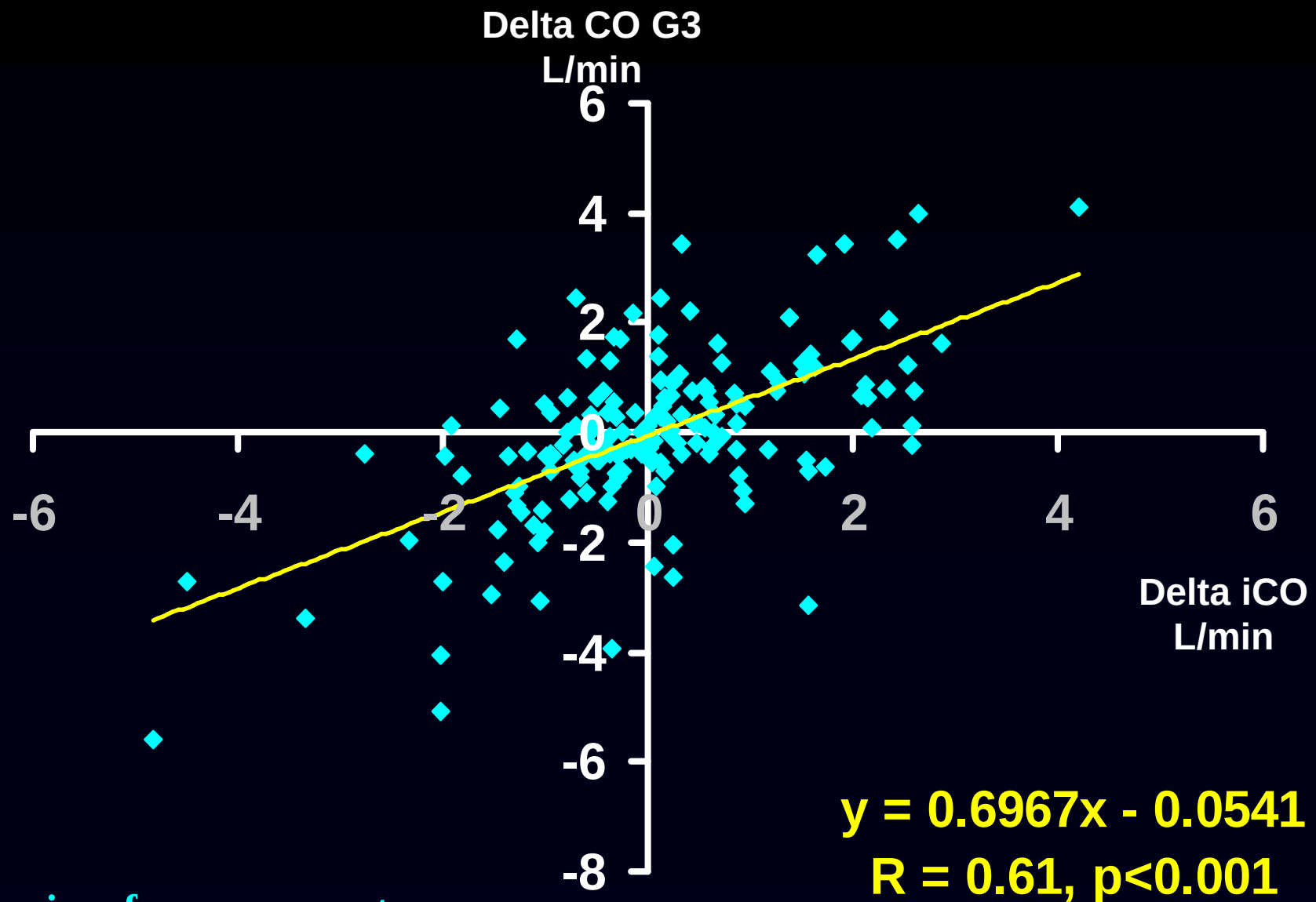
Changes in CO cannot be predicted from changes in arterial pressure



Reference method

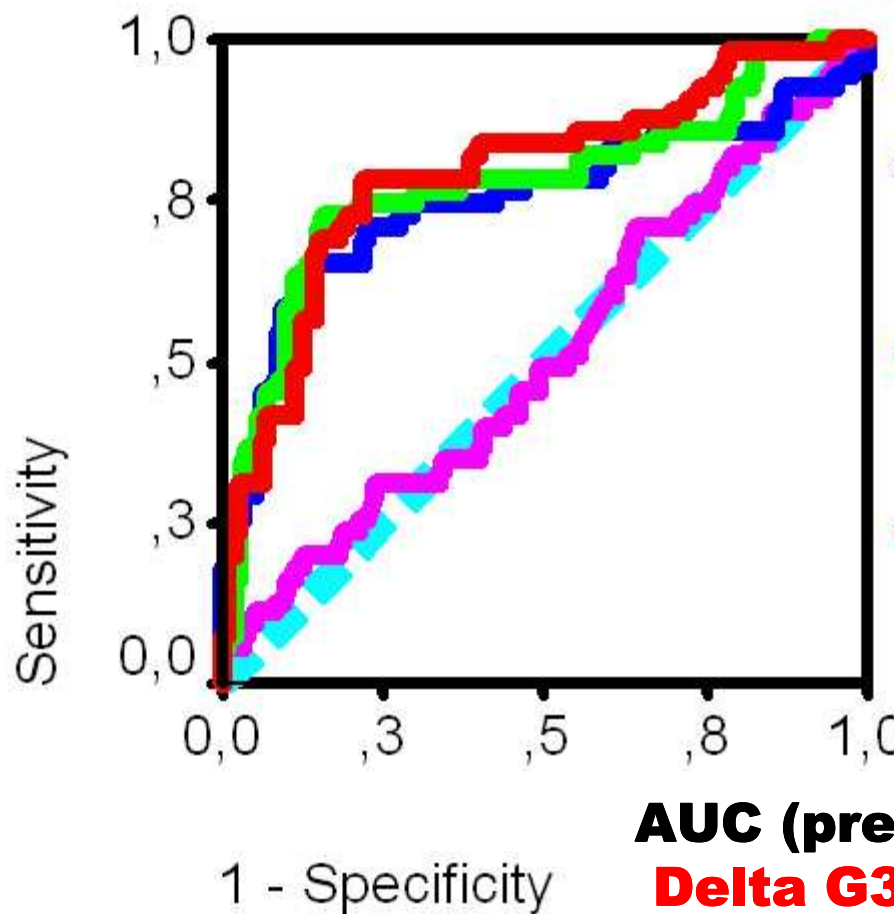
183 pairs of measurements
56 pts

Changes in CO are adequately detected by FloTrac G3



183 pairs of measurements
56 pts

ROC Curve



183 pairs of measurements
56 pts

AUC (prediction of a 15% change in iCO):

Delta G3 %: **0.794 (0.719-0.870)**

Delta G2 %: **0.777 (0.694-0.860)**

Delta CCO %: **0.751 (0.661-0.842)**

Delta MAP %: **0.512 (0.419-0.605)**

Conclusions

- **Pulse contour methods reliably estimate cardiac output in most instances.**
- **Depending on the algorithm, calibration may be required.**
- **The choice of the method should be guided by patients characteristics and the potential interest (need?) for additional measurements.**